

NMR STUDY OF THE DYNAMIC PROPERTIES OF BONE WATER



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INTRODUCTION

Water plays a pivotal role in the biology of bone. It serves as a solvent for transport of nutrients to and from osteocytes and largely determines the bone's viscoelastic properties. Despite its importance, the nature and binding properties of bone water are incompletely understood. Fernandez et al [2,3], were able to measure water diffusion in solid bone, by studying the H₂O/D₂O exchange kinetics, suggesting the presence of two water components of widely differing diffusion rate.

OBJECTIVES

• To investigate the properties of the two bone water fractions by monitoring the



NMR signal while the water is gradually expelled by dehydrating the bone at elevated temperature.

 To further validate these results by thermogravimetric analysis (TGA) - following the mass of the bone as a function of heating time.

METHODS AND MATERIALS

Sample: rectangular section (10×4×1mm³) of cortical bone, with the marrow removed, harvested from the mid-shaft of the tibia of a 14 week old New Zealand white rabbit.

NMR Experiment:

- the sample was placed in a 5mm NMR tube with no lid in the spectrometer and maintained at 100°C for 48 hours.
- vertical-bore spectrometer operating at 9.4T (DMX-400, Bruker)
- after 20 minutes, to allow equilibration, the FID (30 scans, 20° flip angle = 1.72 s, T_B = 1.5s, dwell time = 5 s) was acquired over 48 hours (every 5, 15 and 60 minutes for time periods 0-1, 1-6 and 6-48 hours).
- T₁ was measured with inversion recovery at various times throughout the 48 hours (Table 2, τ_{90} = 7.75 \mathbb{K} s, $\tau_{180} = 15.5 \mathbb{K}$ s, $T_1 = 0.1 - 3s$).

TGA Experiment:

• the sample was placed in the TGA machine and



hours while the FID and T₁

of the bone water are

measured periodically.

Figure 3: Results from NMR A Signal from bone water as a function of drying time for each component. All three curves show a two-stage behaviour, with the transition occuring around 6 hours after the start of heating. **B**, **C** time course of long (**B**) and short (**C**) T_2^* components compared with finite element simulations.



- heated to 100°C for 15 hours.
- the total mass and heat flow into/out of the sample were measured as a function of heating time.

Data Analysis:

are both water.

- Each FID was fitted to a biexponential function of the form $M_1 \exp\{-t / T_2^*(1)\} + M_2$ $\exp\{-t / T_2(2)\}$
- Diffusion constants were calculated by modelling the bone as a one-dimensional object of length d and diffusion constant, D. In this case the signal, I(t), at long times is given by $l(t) \approx 8 l(0)/p^2 \exp\{-Dp^2 t / d^2\}$ [4].
- Finite element simulations were run based on the same one dimensional model using the calculated values of D and I(0) (Figure 3).



13.3 hours.

DISCUSSION

- All the FIDs decay in a biexponential fashion with $T_2^* = 6.5$ and 250 is (Figure 2)
- T_1 was similar for both components and increased with drying time (Table 2). This change reflects reduced H_2O-H_2O interaction as the water content falls.
- All the decay curves (Figure 3) followed a two-stage behaviour with the transition point between the two stages being around 6 hours.
- Despite this unexpected result, the decay of each stage is approximately monoexponential enabling diffusion coefficients to be calculated using [4].
- The results (Table 1) show that the long T_2^* component is more mobile than the short T_2^* component, consistent with their assignments as free and bound water.
- Simulations using these values of D are in good agreement with experiment for

Time /	ms
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Figure 2: The FID of bone water at 100°C shows distinct biexponential decay which we associate with two water components. The short T_2^* component (T_2^* = 6.5 \mathbb{K} s) corresponds to protein bound water, while the long T_2^* component (T_2^* = 250 🕅 s) is associated with 'free' water in the pore space.

			_
D / 10 ⁻⁷ cm ² s ⁻¹			Table 1: D
Component	1 st stage	2 nd stage	of each w each stac
Total signal	6.50	0.45	process.
Short T_2^*	1.83	0.27	water whic
Long T_2^{\star}	7.17	0.50	cm ² s ⁻¹ just
Table 2: T₁ of rem water as a function time at 100°C.	naining bone ion of drying	Time / hours	Short T ₂
components inc	reases with	0	0.841
heating time due	to decreased	5.6	0.9865
H ₂ O-H ₂ O interactio	n. Note also	21.5	1.2149
similar T ₁ suggest	ing that they	27.4	1.2899

iffusion constants ater component at ge of the drying Compared with bulk h has D ~8.0 × 10⁻⁵ below 100°C.

Time / hours	T ₁ / s		
	Short T ₂ *	Long T ₂ *	
0	0.841	0.8397	
5.6	0.9865	0.9855	
21.5	1.2149	1.2019	
27.4	1.2899	1.329	
45.5	1.3656	1.4532	

each stage and each component (Figure 3 B,C).

 Thermogravimetric analysis suggests that the two-stage behaviour is repeatable and that the change between stages is accompanied by an exothermic reaction.

 It is likely that the two-stage behaviour is dependent on complex binding properties of water and is suggested that it could involve collagen denaturing, a process that occurs around 70°C.

CONCLUSIONS

Time-resolved NMR experiments during drying of bone can provide insight into the dynamics of water in different binding states.

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