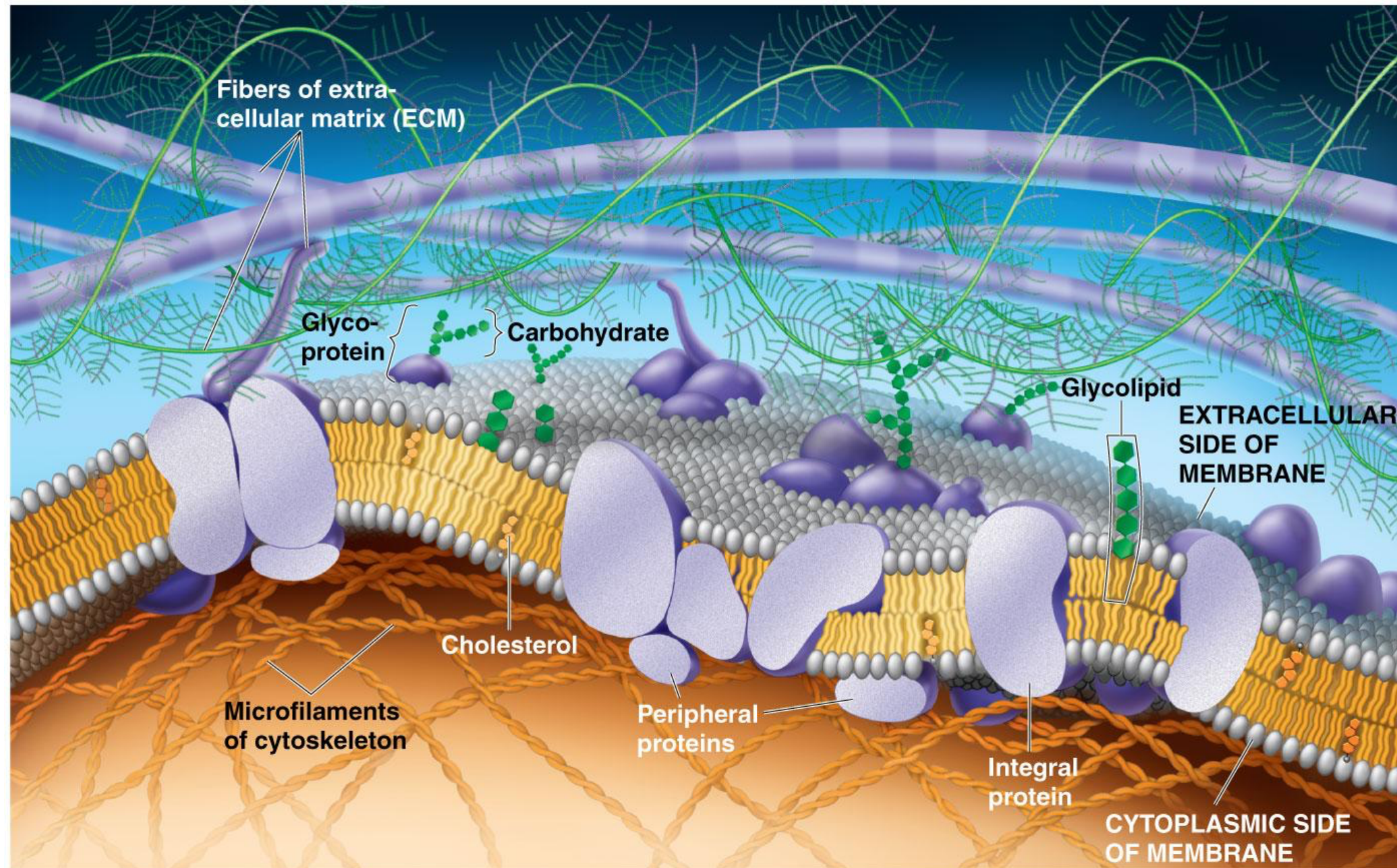


MAE 545: Lectures 12,13 (3/27)

Osmotic pressure and mechanics of cell membranes



Gibbs free energy

$$G = E + pV - TS = \sum_i N_i \mu_i$$

energy

pressure,
volume

temperature,
entropy

chemical
potential of
component i

Entropy

$$S = k_B \ln \Omega$$

Boltzmann
constant

number of
configurations

Derivatives of system energy

$$dE = TdS - pdV + \sum_i \mu_i dN_i$$

$$T = \left(\frac{\partial E}{\partial S} \right)_{V, N_i} \quad p = - \left(\frac{\partial E}{\partial V} \right)_{S, N_i}$$

$$\mu_i = \left(\frac{\partial E}{\partial N_i} \right)_{S, V}$$

Derivatives of Gibbs free energy

$$dG = -SdT + Vdp + \sum_i \mu_i dN_i$$

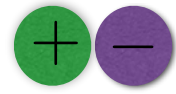
$$S = - \left(\frac{\partial G}{\partial T} \right)_{p, N_i} \quad V = \left(\frac{\partial G}{\partial p} \right)_{T, N_i}$$

$$\mu_i = \left(\frac{\partial G}{\partial N_i} \right)_{T, p}$$

**In thermodynamic equilibrium
system minimizes Gibbs free
energy, when temperature T
and pressure p are fixed!**

Charge dissociation in solution

example
NaCl salt



binding energy

$$-E_b$$

entropy

$$k_B \ln v_0 \leftarrow \begin{array}{l} \text{some} \\ \text{characteristic} \\ \text{volume} \end{array}$$

interaction energy

$$\approx 0$$

entropy

$$k_B \ln(V/N)$$

volume of the
whole system

number of
dissociated pairs

Free energy change for charge dissociation

$$\Delta G = \Delta E - T\Delta S = E_b - k_B T \ln(V/Nv_0)$$

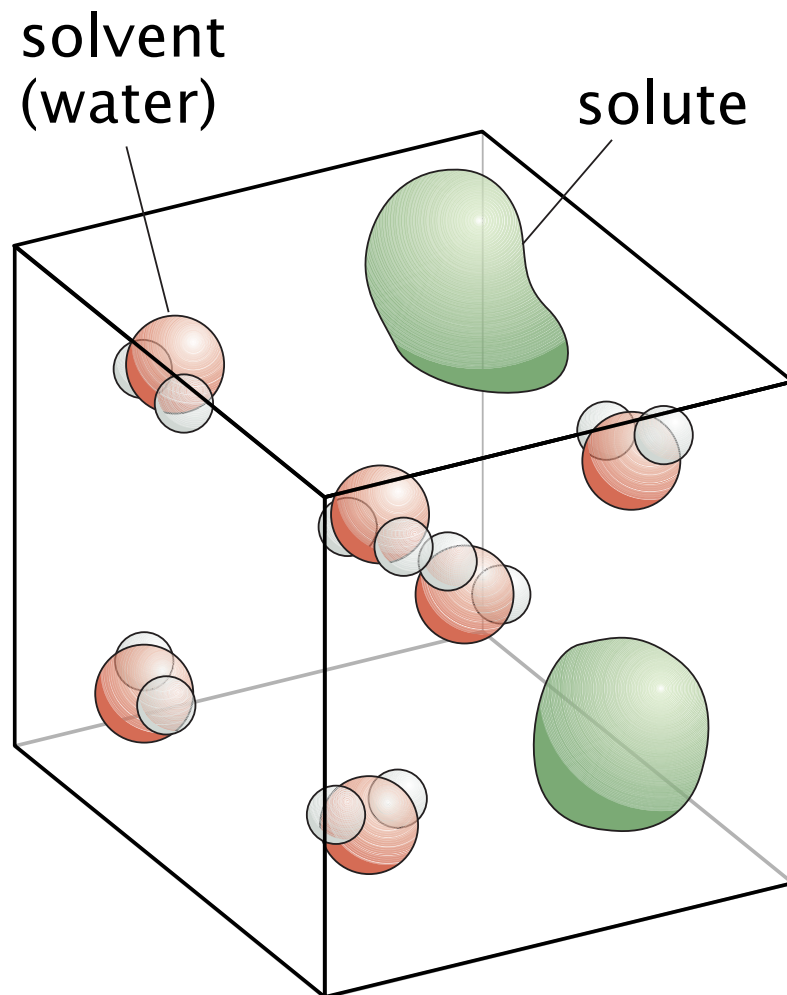
In thermodynamic equilibrium $\Delta G = 0$

$$c = \frac{N}{V} = \frac{1}{v_0} e^{-E_b/k_B T}$$

concentration of dissociated ions

**Entropy is the reason why
many molecules dissociate
and ionize in solution!**

Free energy of dilute solutions



Ideal solution: interactions between solute particles are negligible

Gibbs free energy of ideal solution

$$G = N_{\text{H}_2\text{O}}\mu_{\text{H}_2\text{O}}^0 + N_s\epsilon_s - TS_{\text{mix}}$$

**water free
energy**

**solute
energy**

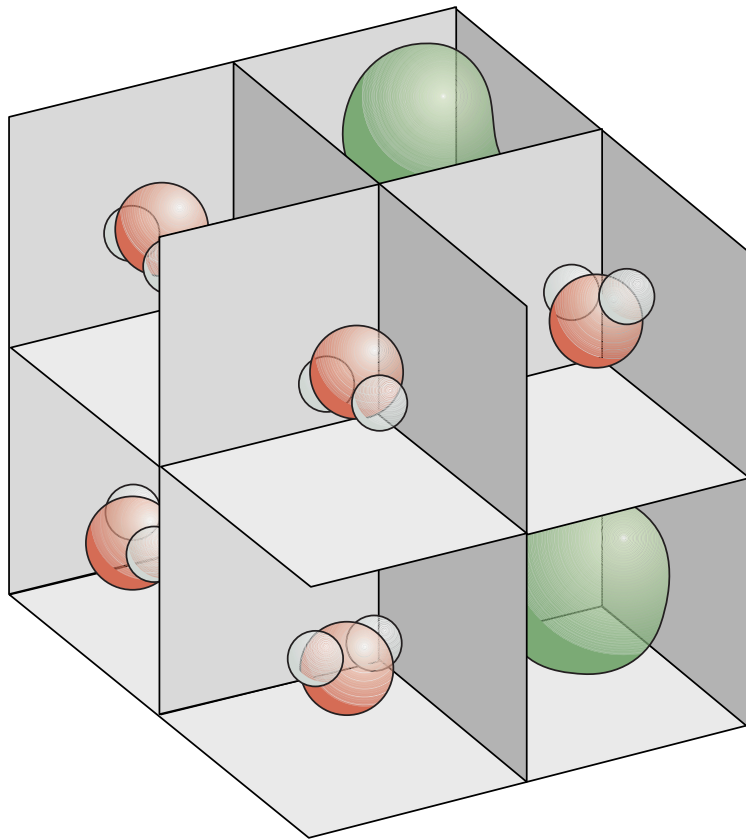
**mixing
entropy**

Figure from R. Phillips et al.,
Physical Biology of the Cell

Mixing entropy of dilute solutions

Let's divide volume in small boxes each containing one water molecule or one solute molecule.

How many different configurations of water and solute molecules are possible?



$$\Omega = \binom{N_{\text{H}_2\text{O}} + N_s}{N_s} = \frac{(N_{\text{H}_2\text{O}} + N_s)!}{N_{\text{H}_2\text{O}}! N_s!}$$

$$S_{\text{mix}} = k_B \ln \Omega$$

Stirling approximation

$$\ln N! \approx N \ln N$$

$$S_{\text{mix}} \approx k_B \left[N_{\text{H}_2\text{O}} \ln \left(\frac{N_{\text{H}_2\text{O}} + N_s}{N_{\text{H}_2\text{O}}} \right) + N_s \ln \left(\frac{N_{\text{H}_2\text{O}} + N_s}{N_s} \right) \right]$$

Small number of solute particles $N_s \ll N_{\text{H}_2\text{O}}$

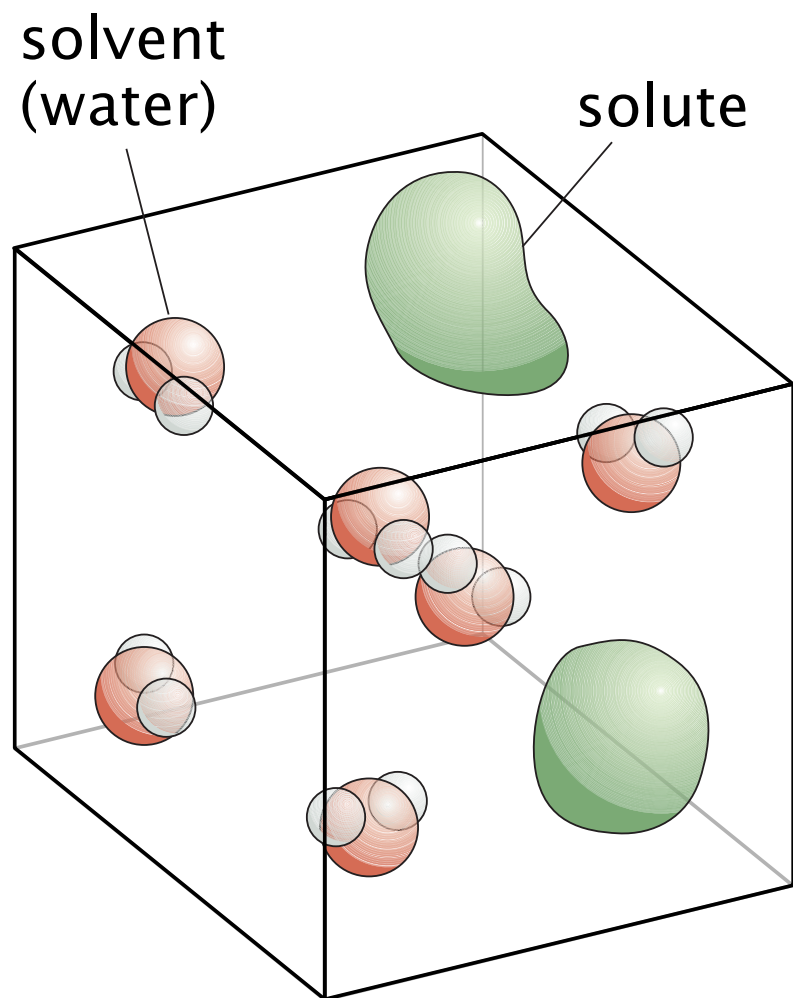
$$S_{\text{mix}} \approx k_B \left[N_s - N_s \ln \left(\frac{N_s}{N_{\text{H}_2\text{O}}} \right) \right]$$

Figure from R. Phillips et al.,
Physical Biology of the Cell

Chemical potentials in dilute solution

$$G = N_{\text{H}_2\text{O}}\mu_{\text{H}_2\text{O}}^0 + N_s\epsilon_s - TS_{\text{mix}}$$

$$G \approx N_{\text{H}_2\text{O}}\mu_{\text{H}_2\text{O}}^0 + N_s\epsilon_s + k_B T \left[N_s \ln \left(\frac{N_s}{N_{\text{H}_2\text{O}}} \right) - N_s \right]$$



Chemical potential of solute

$$\mu_s = \frac{\partial G}{\partial N_s} = \epsilon_s + k_B T \ln \left(\frac{N_s}{N_{\text{H}_2\text{O}}} \right)$$

$$\mu_s(T, p, c_s) = \epsilon_s(T, p) + k_B T \ln(c_s v)$$

solute concentration
volume occupied by
one water molecule

$$c_s = N_s/V$$

$$v = V/N_{\text{H}_2\text{O}}$$

Chemical potential of water

$$\mu_{\text{H}_2\text{O}} = \frac{\partial G}{\partial N_{\text{H}_2\text{O}}} = \mu_{\text{H}_2\text{O}}^0 - k_B T \frac{N_s}{N_{\text{H}_2\text{O}}}$$

$$\mu_{\text{H}_2\text{O}}(T, p, c_s) = \mu_{\text{H}_2\text{O}}^0(T, p) - k_B T c_s v$$

Figure from R. Phillips et al.,
Physical Biology of the Cell

Osmotic pressure

Small water molecules can pass through a semipermeable membrane, which blocks large solute macromolecules.

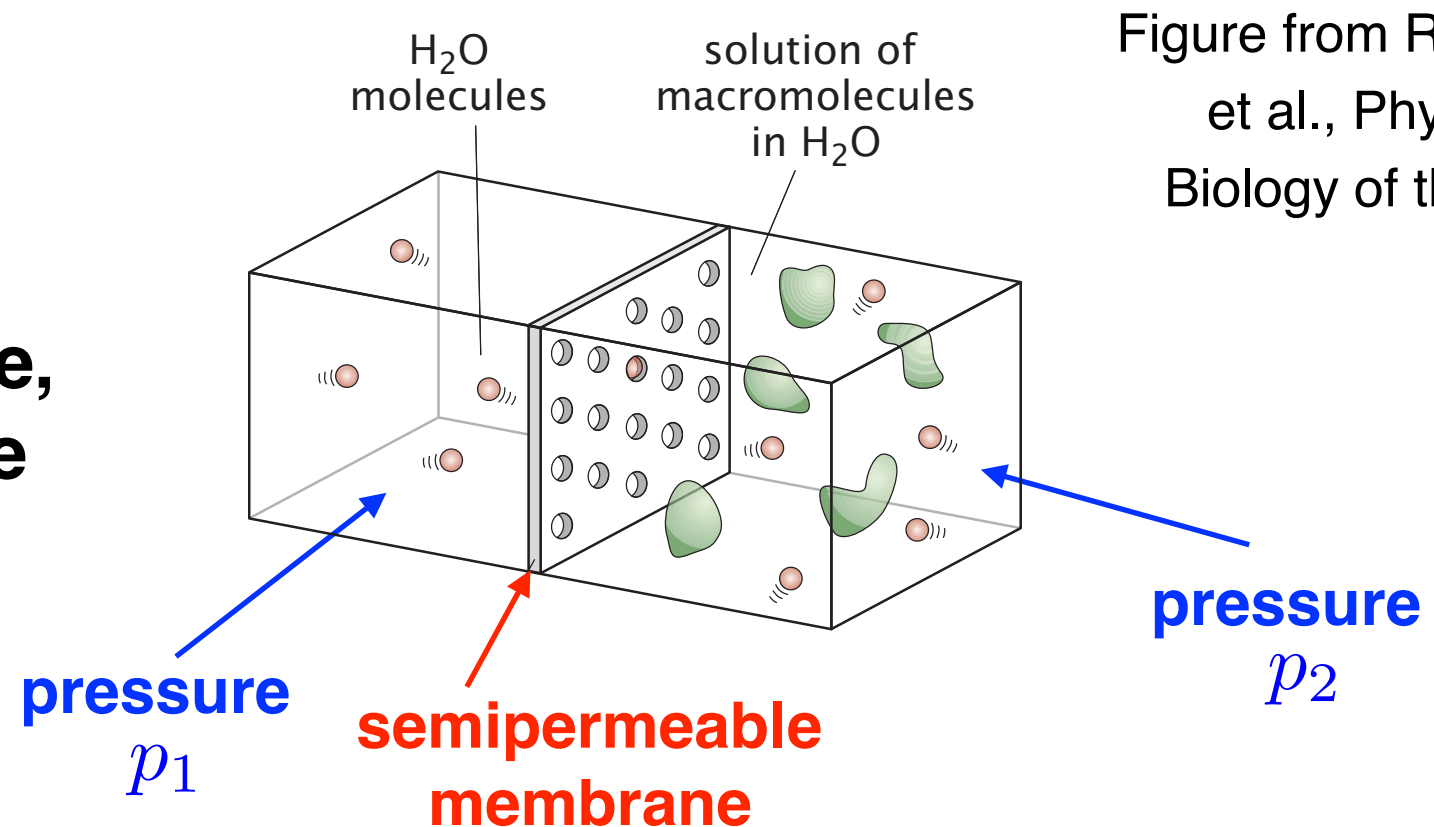


Figure from R. Phillips
et al., Physical
Biology of the Cell

$$G = N_1 \mu_{\text{H}_2\text{O}}(T, p_1, 0) + N_2 \mu_{\text{H}_2\text{O}}(T, p_2, c_s) + N_s \mu_s(T, p_2, c_s)$$

In thermodynamic equilibrium the Gibbs free energy G is minimized, which means that chemical potentials of water are the same on both sides of the semipermeable membrane!

$$\mu_{\text{H}_2\text{O}}(T, p_1, 0) = \mu_{\text{H}_2\text{O}}(T, p_2, c_s)$$

Osmotic pressure

Water flows from region of low concentration of macromolecules to region of large concentrations. This additional water increases pressure and the water stops flowing once the osmotic pressure is reached.

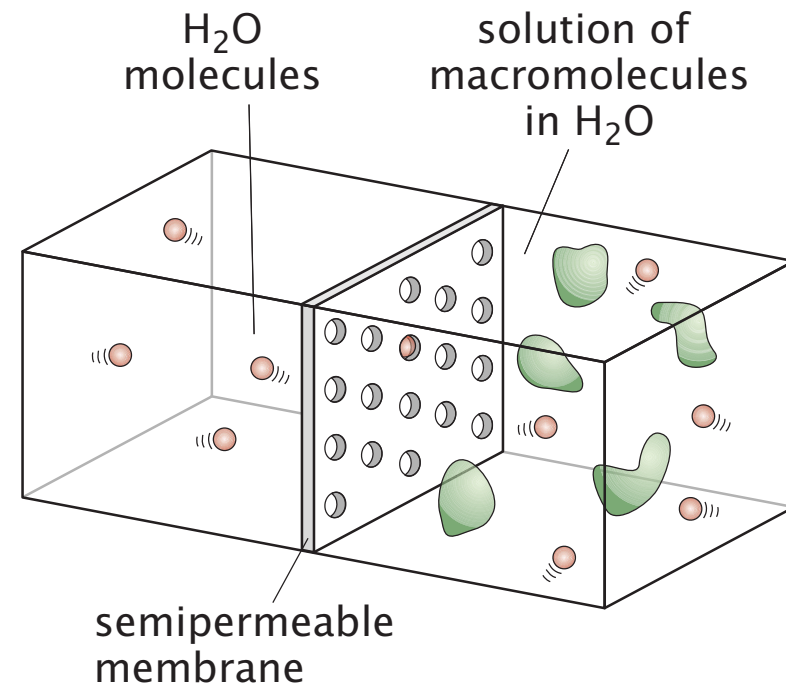


Figure from R. Phillips
et al., Physical
Biology of the Cell

$$\mu_{\text{H}_2\text{O}}(T, p_1, 0) = \mu_{\text{H}_2\text{O}}(T, p_2, c_s)$$

$$\mu_{\text{H}_2\text{O}}(T, p_2, c_s) = \mu_{\text{H}_2\text{O}}^0(T, p_2) - k_B T c_s v$$

$$\mu_{\text{H}_2\text{O}}(T, p_2, c_s) \approx \mu_{\text{H}_2\text{O}}^0(T, p_1) + \left(\frac{\partial \mu_{\text{H}_2\text{O}}^0}{\partial p} \right) (p_2 - p_1) - k_B T c_s v$$

$$\Pi = p_2 - p_1 = k_B T \Delta c_s$$

Osmotic pressure depends only on temperature and concentration difference across the membrane!

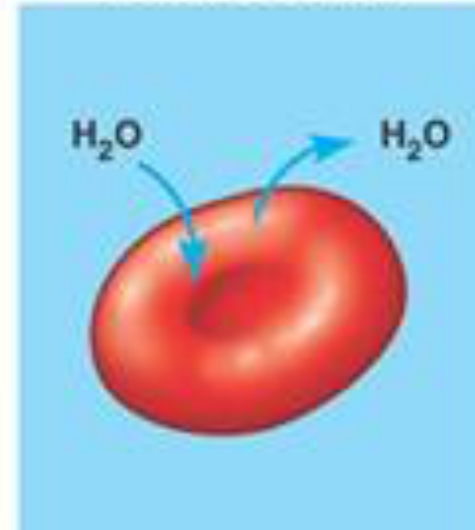
Osmotic pressure in cells

If extracellular solution has different concentration of ions from the interior of cells, then the resulting flow of water can cause the cell to shrink or swell and even burst.



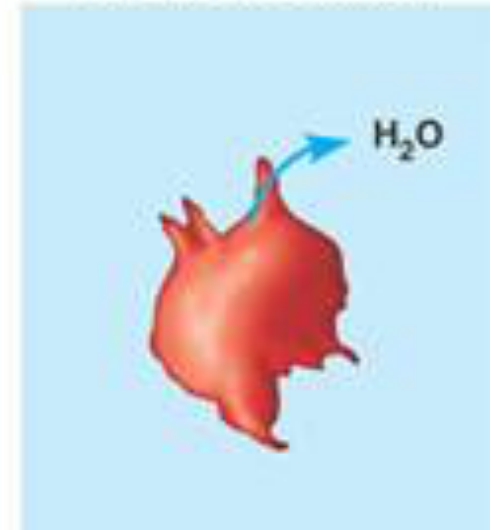
hypotonic
solution

$$C_{s,out} \ll C_{s,in}$$



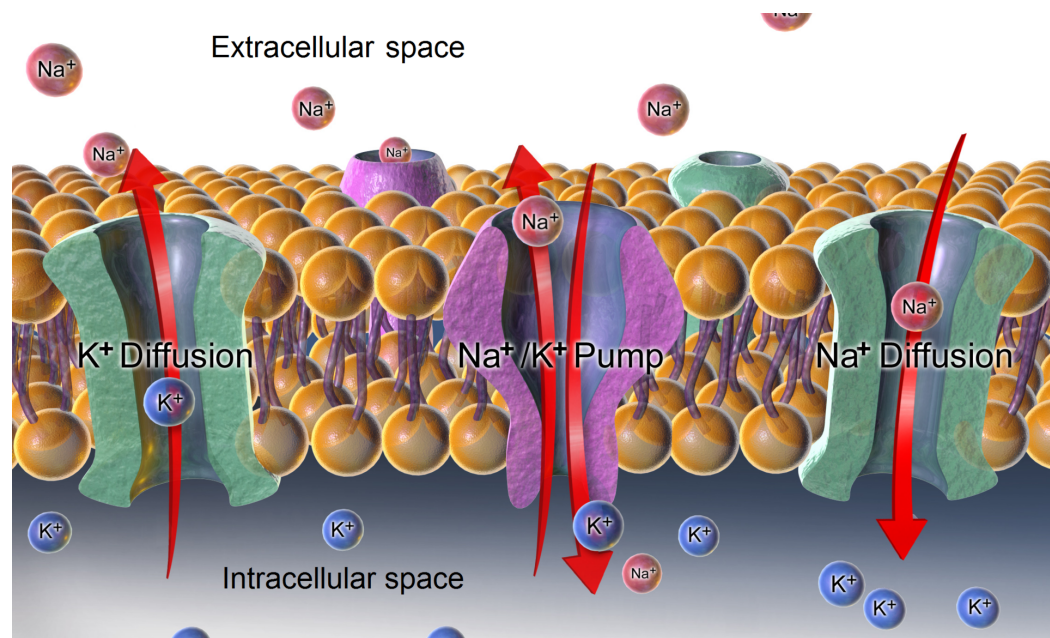
isotonic
solution

$$C_{s,out} \sim C_{s,in}$$



hypertonic
solution

$$C_{s,out} \gg C_{s,in}$$



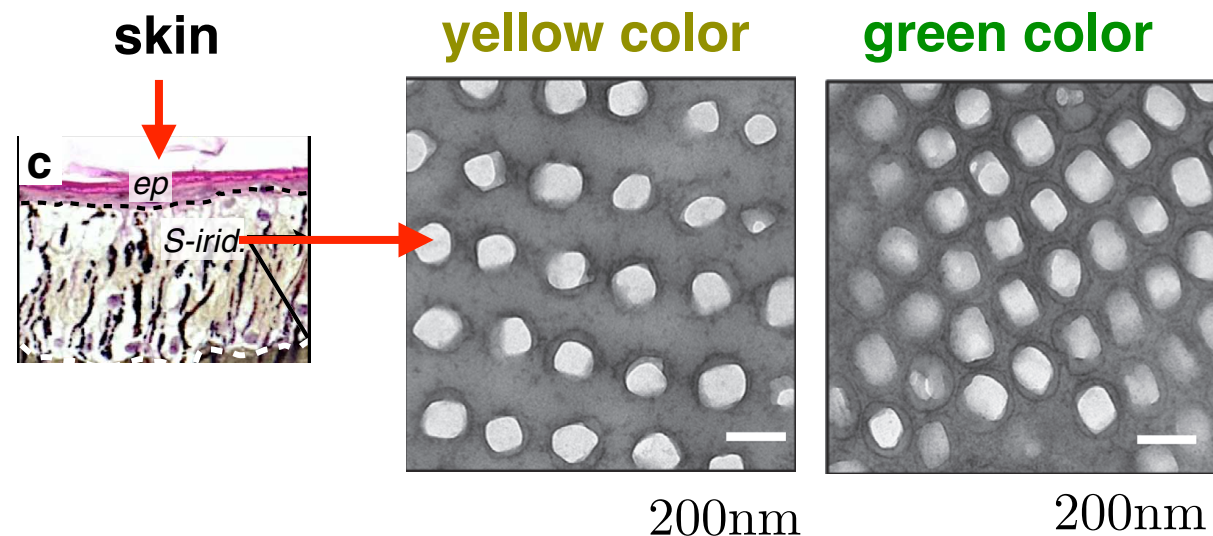
Cells use ion channels and ion pumps to regulate concentration of ions and therefore also the cell volume.

(Note: cell membrane is impermeable for charged particles)

Dynamical structural colors in Chameleon

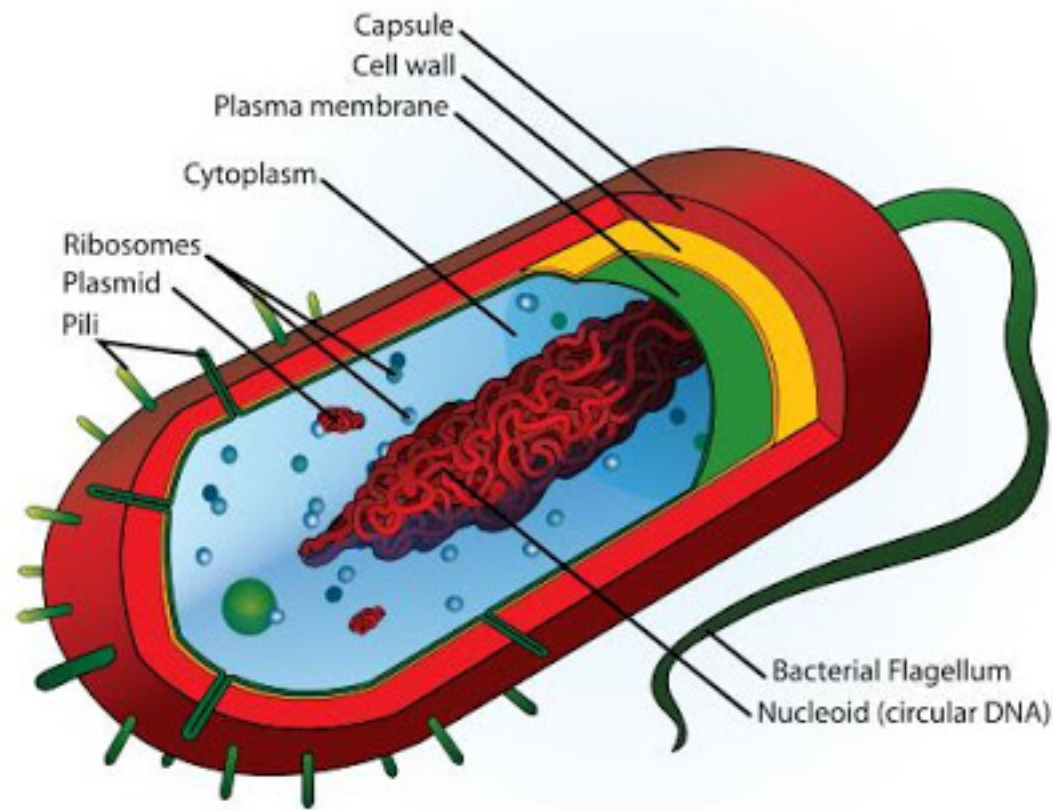


J. Teyssier et al.,
Nat. Comm. 6, 6368 (2015)



Changes in osmotic concentration lead to the swelling of cells in excited chameleon. This changes the spacing of periodic structure from which the ambient light is reflected.

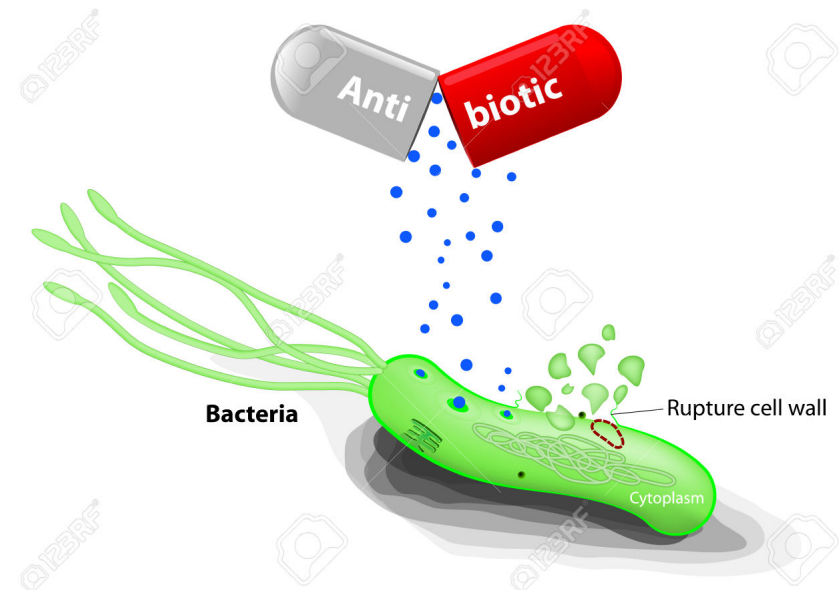
Osmotic pressure in bacteria



Bacteria have strong cell wall that can support large osmotic pressure (Turgor pressure).

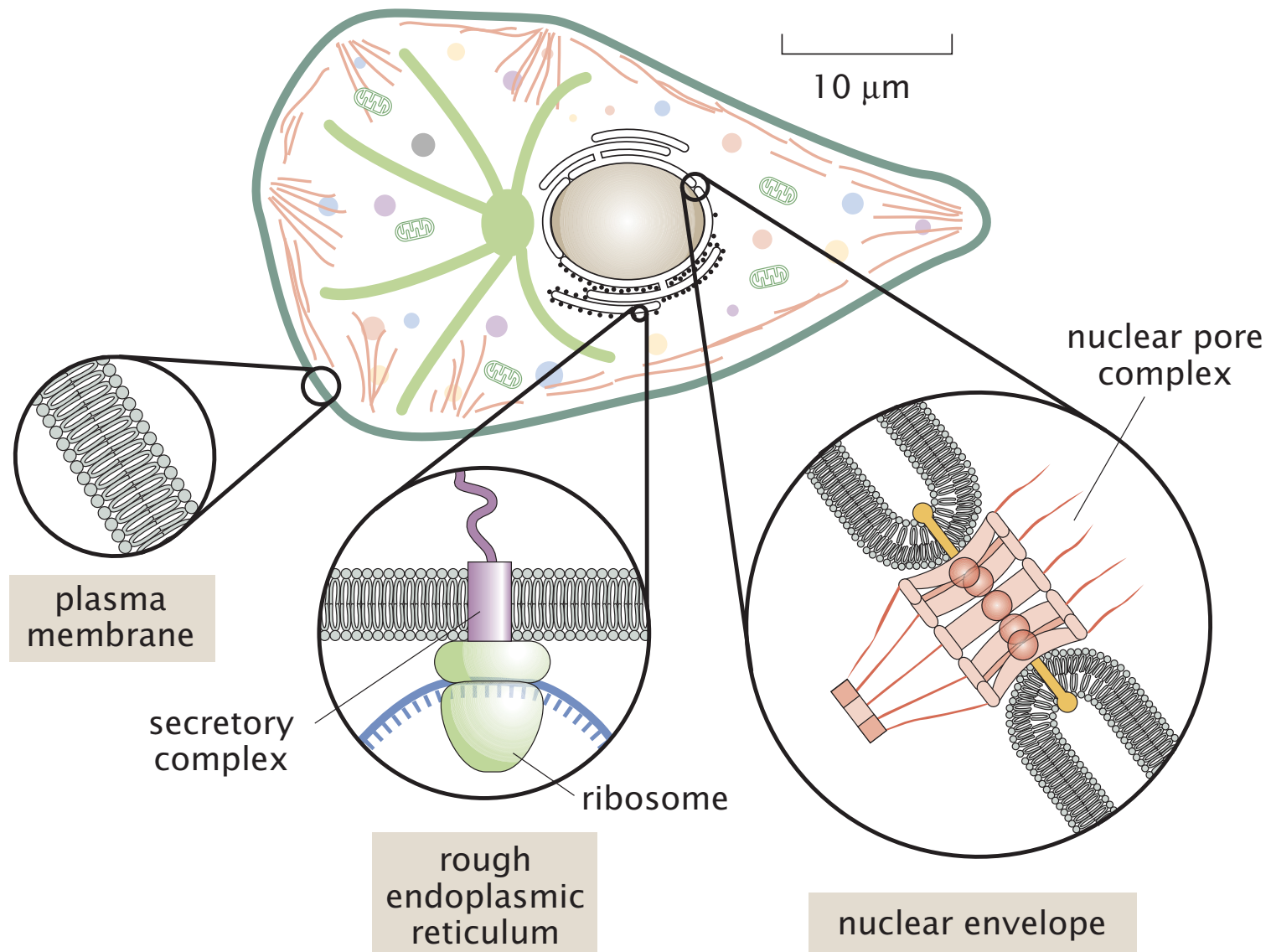
$$\Pi \sim 10^5 \text{ Pa} \sim 1 \text{ bar}$$

Antibiotics cause damage to cell wall and as a result cells rupture due to large Turgor pressure.

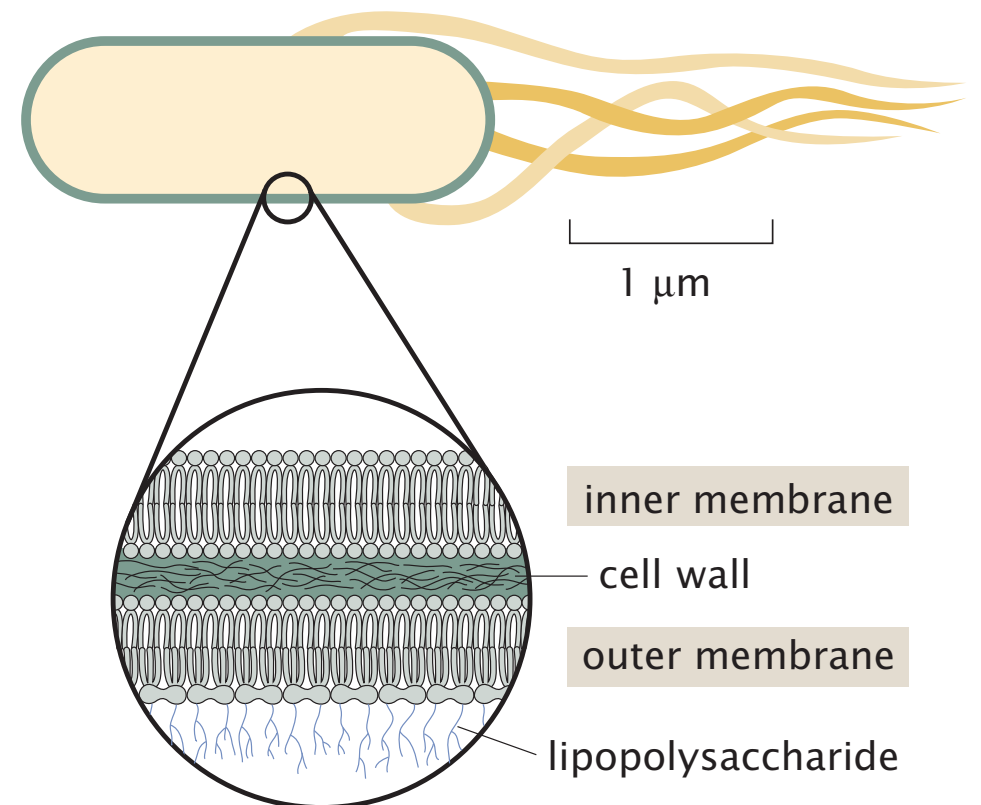


Cell membranes

Eukaryotic cells

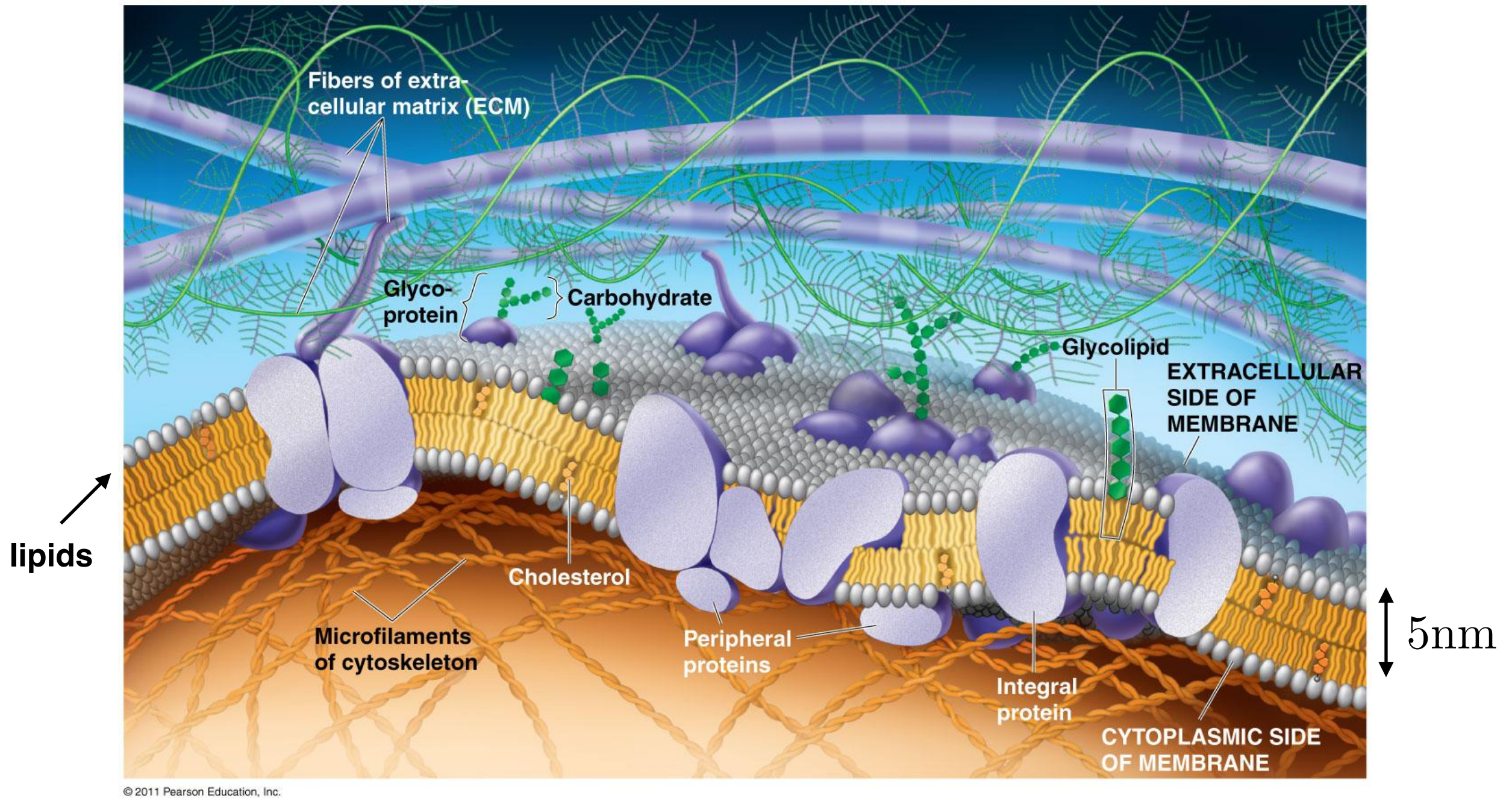


E. Coli

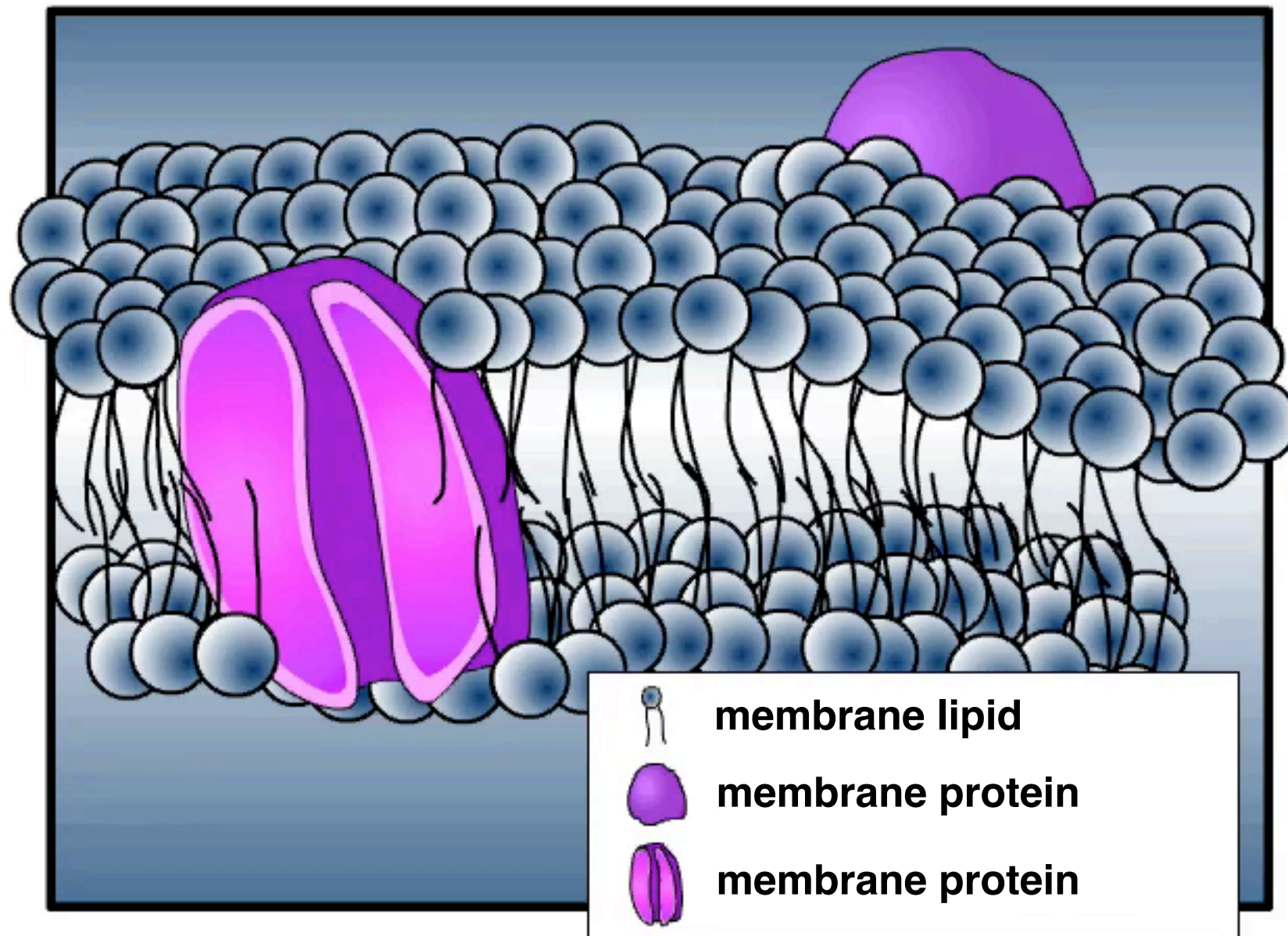


R. Phillips et al., Physical
Biology of the Cell

Cell membrane



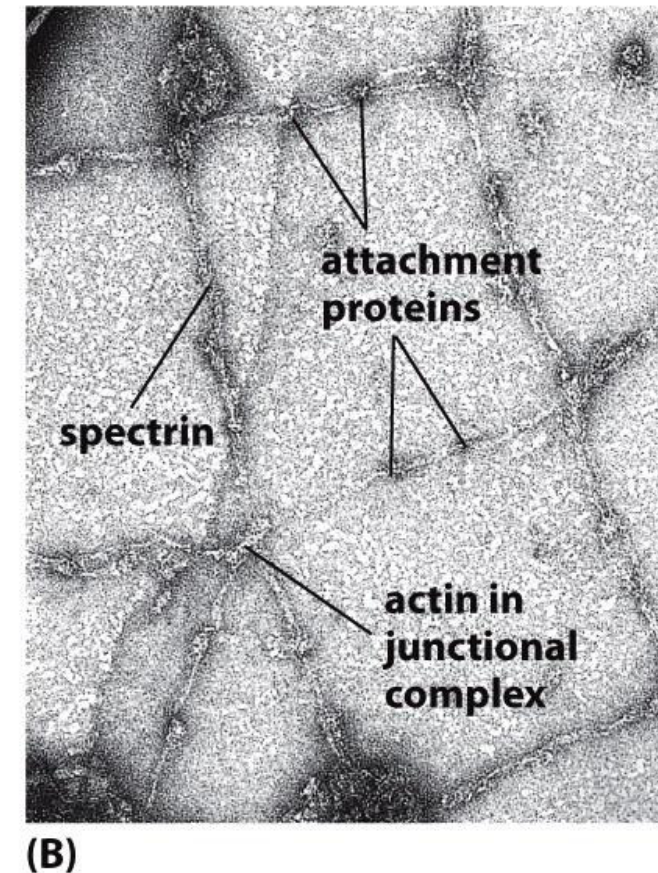
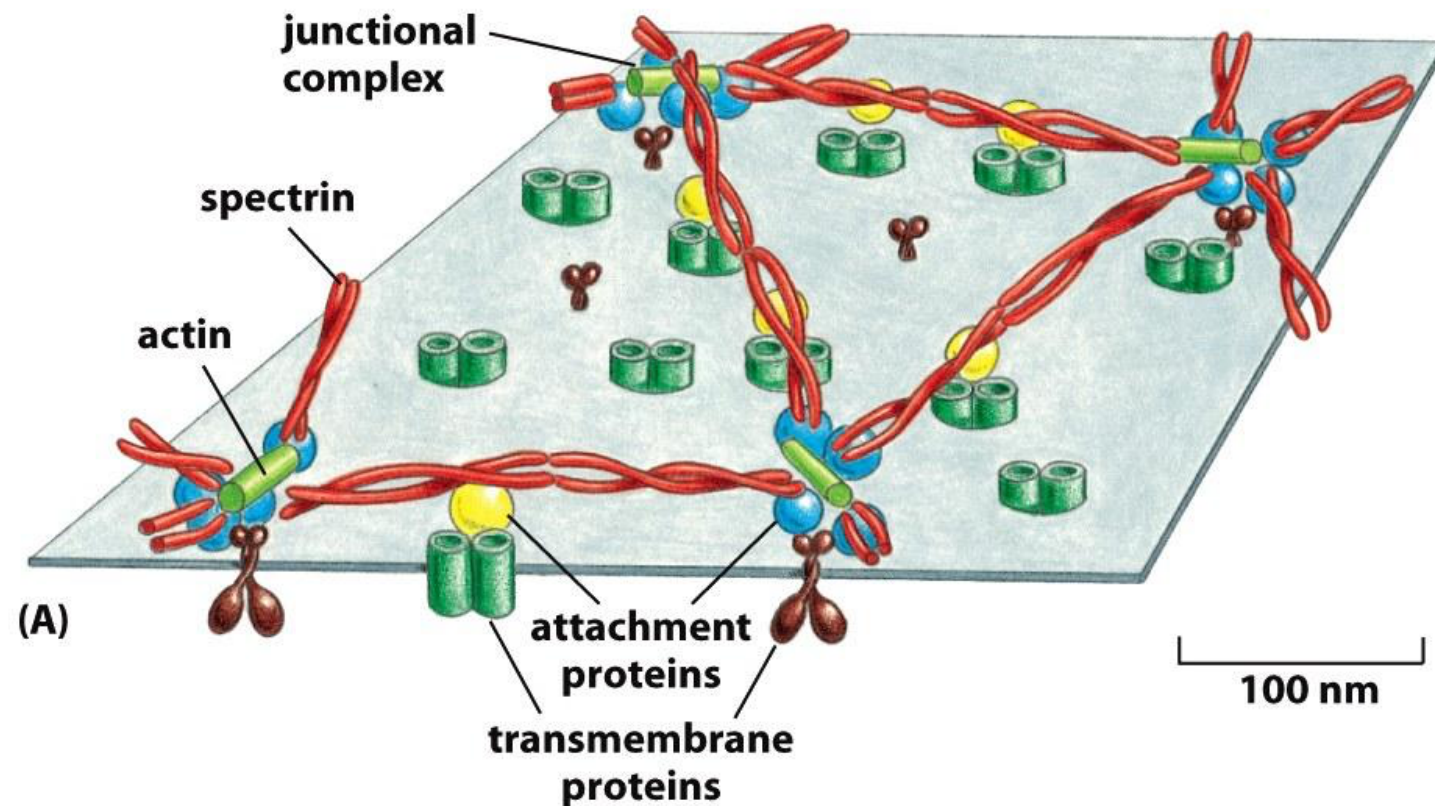
Lipid membrane behaves like fluid



Lipid molecules and proteins can move around!

Flipping of lipid molecules between the layer is unlikely.

Membrane attached spectrin network provides solid-like behavior

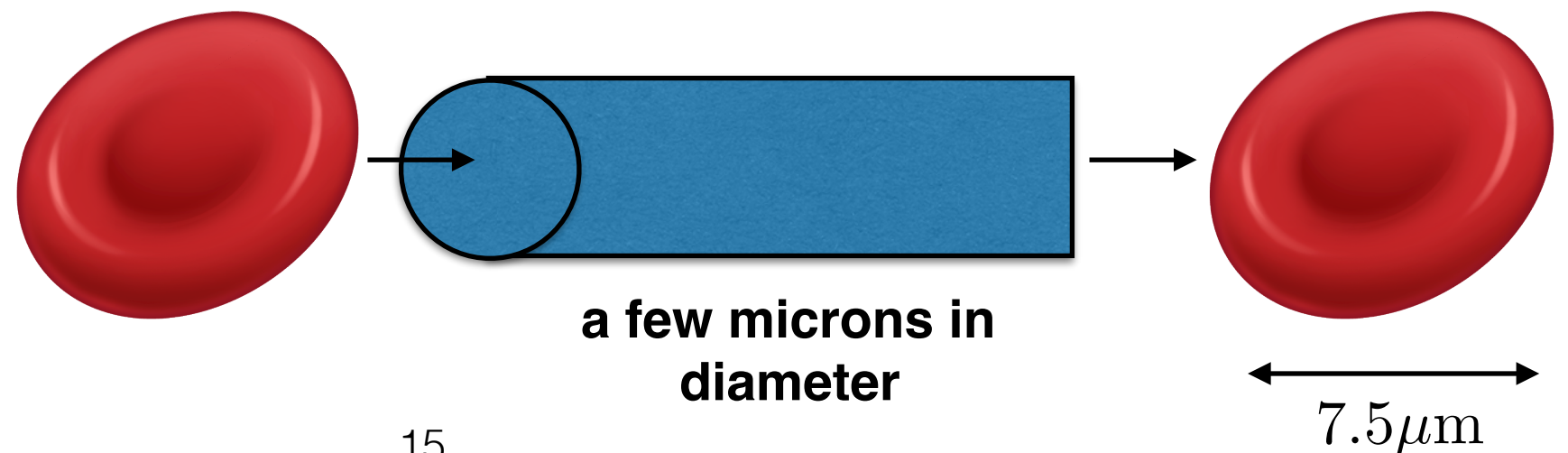


Spectrin network provides structural stability for cells

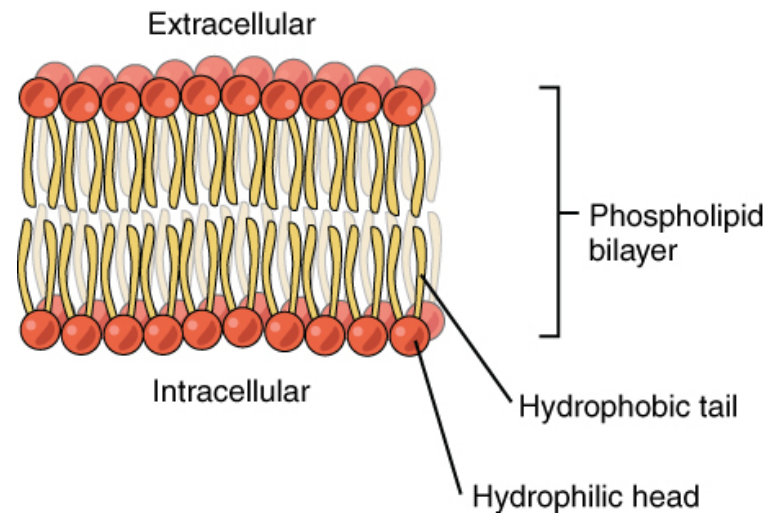
Alberts et al., Molecular Biology of the Cell

red blood cell

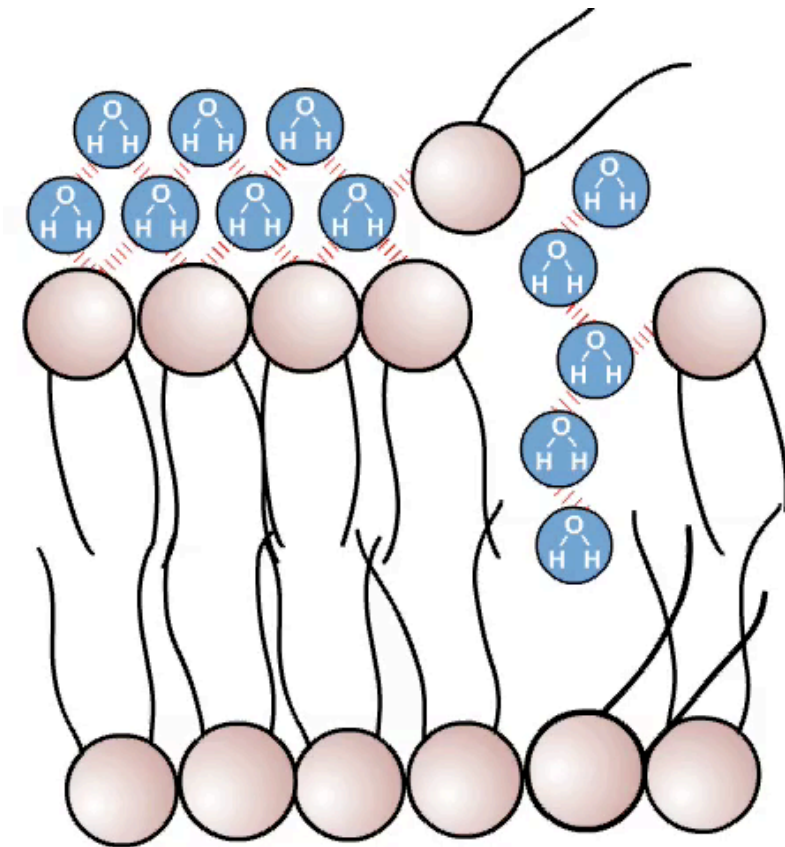
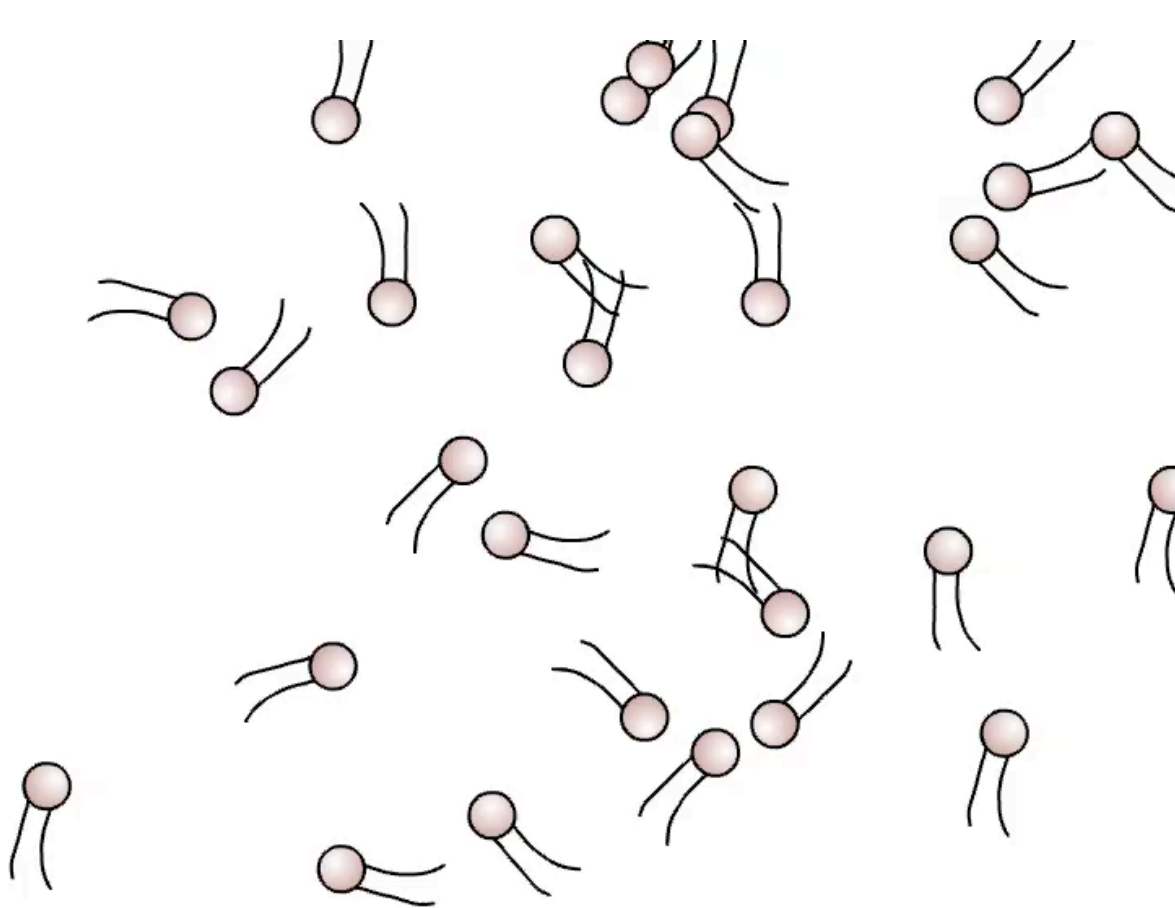
capillary



Lipid membrane

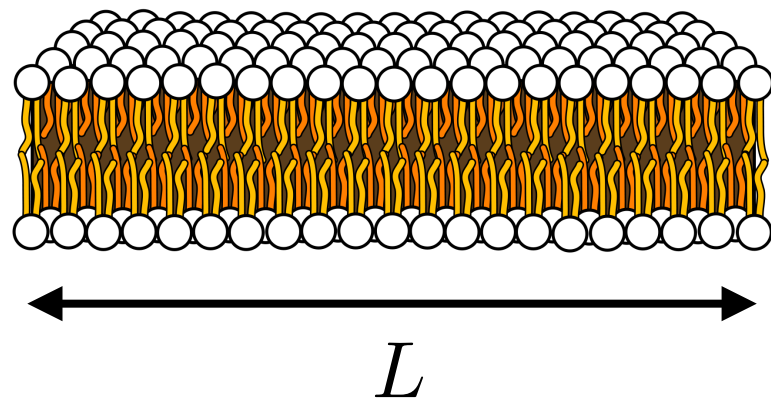


In water solution lipid molecules spontaneously aggregate to prevent undesirable interactions between water and hydrophobic tails.



Flat lipid bilayers vs lipid vesicles

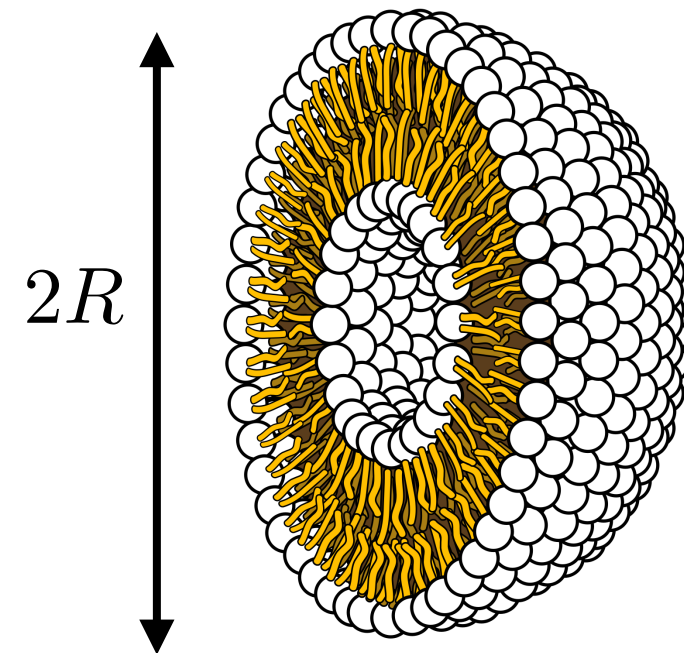
flat bilayer



energy cost on the edge
between lipid tails and
water molecules

$$E \propto L$$

vesicle

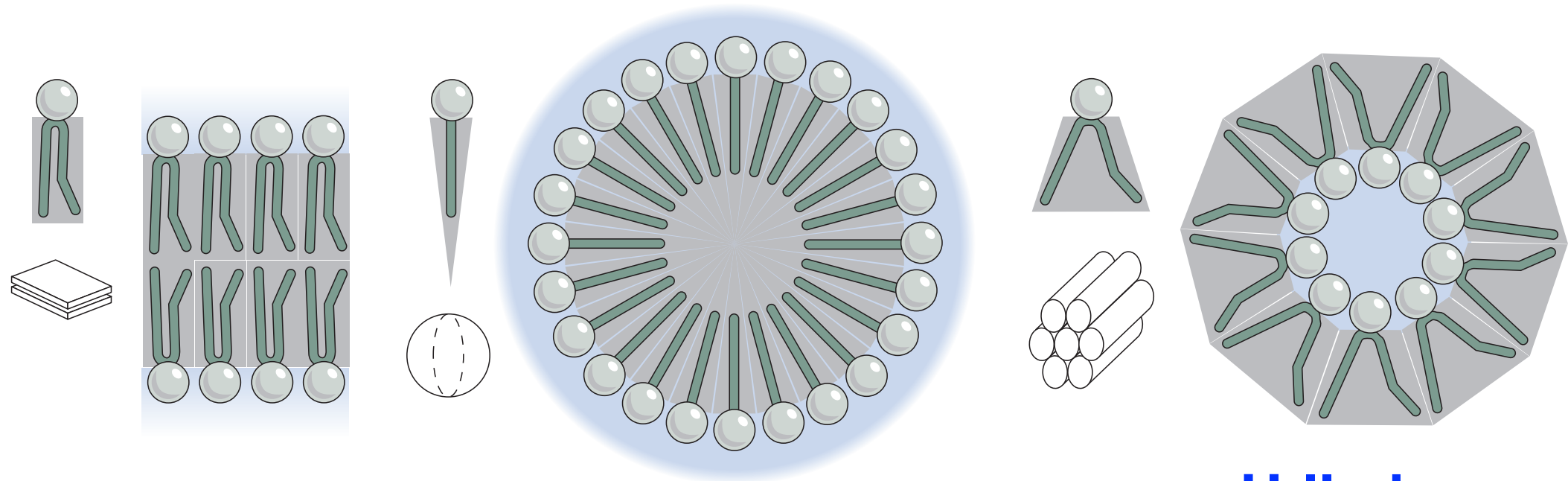


bending energy cost

$$E \propto \text{const}$$

Large vesicles have lower energy cost than flat bilayers!

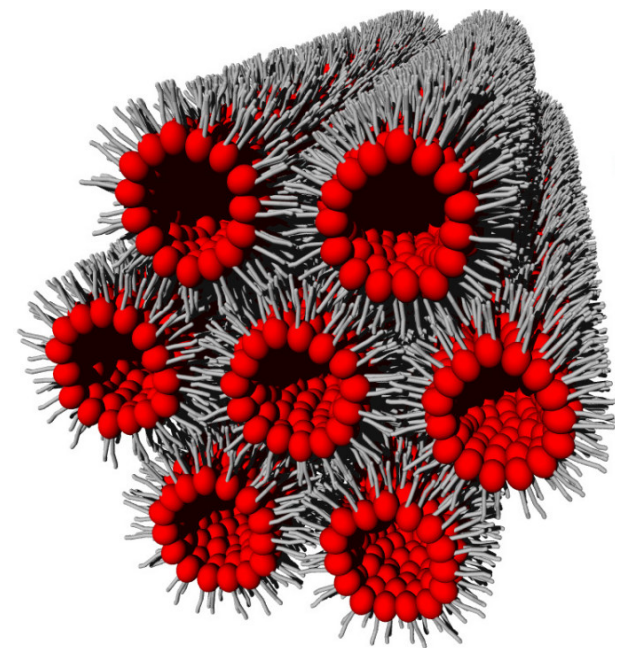
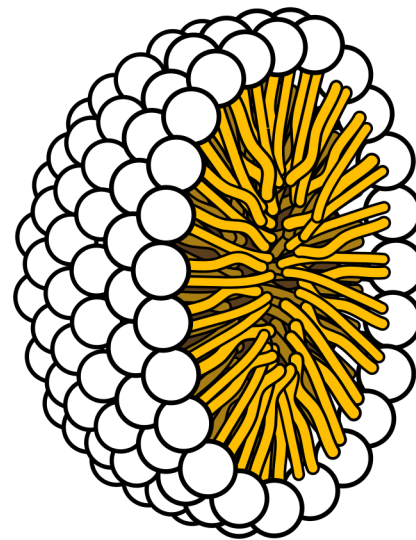
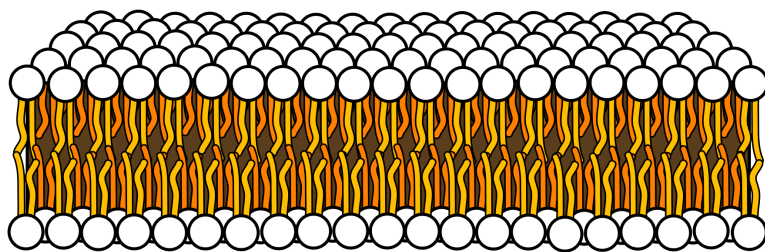
Shape of lipid molecules can induce spontaneous curvature of structures



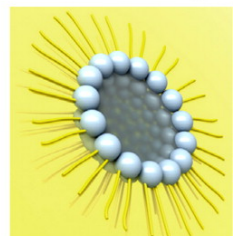
bilayer

micelle

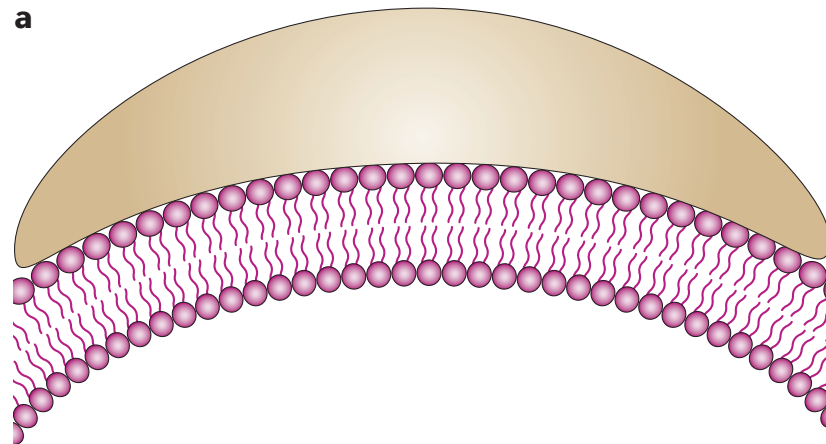
H-II phase



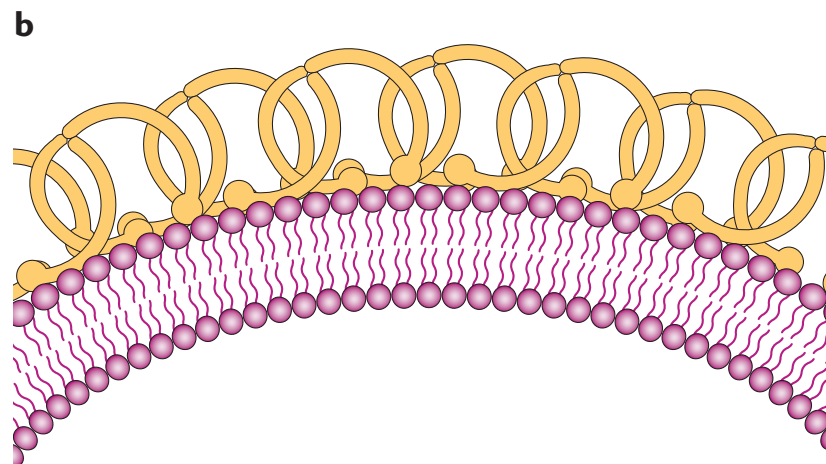
**inverted
micelle**



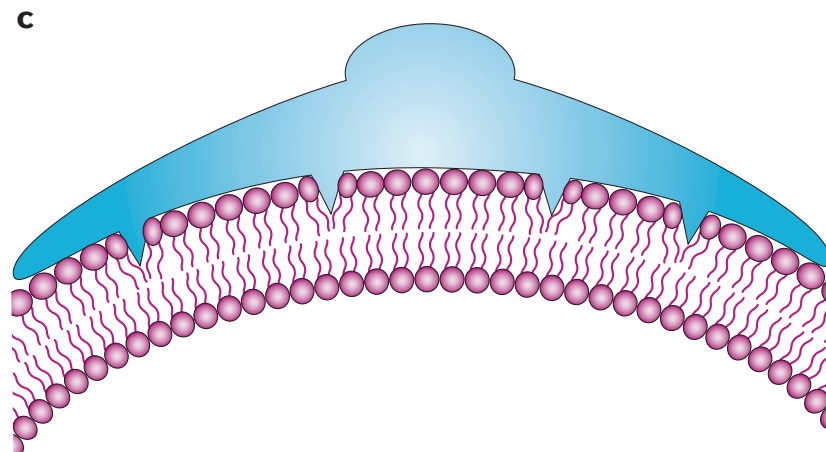
Membrane proteins can induce spontaneous curvature



**binding of rigid
curved proteins**

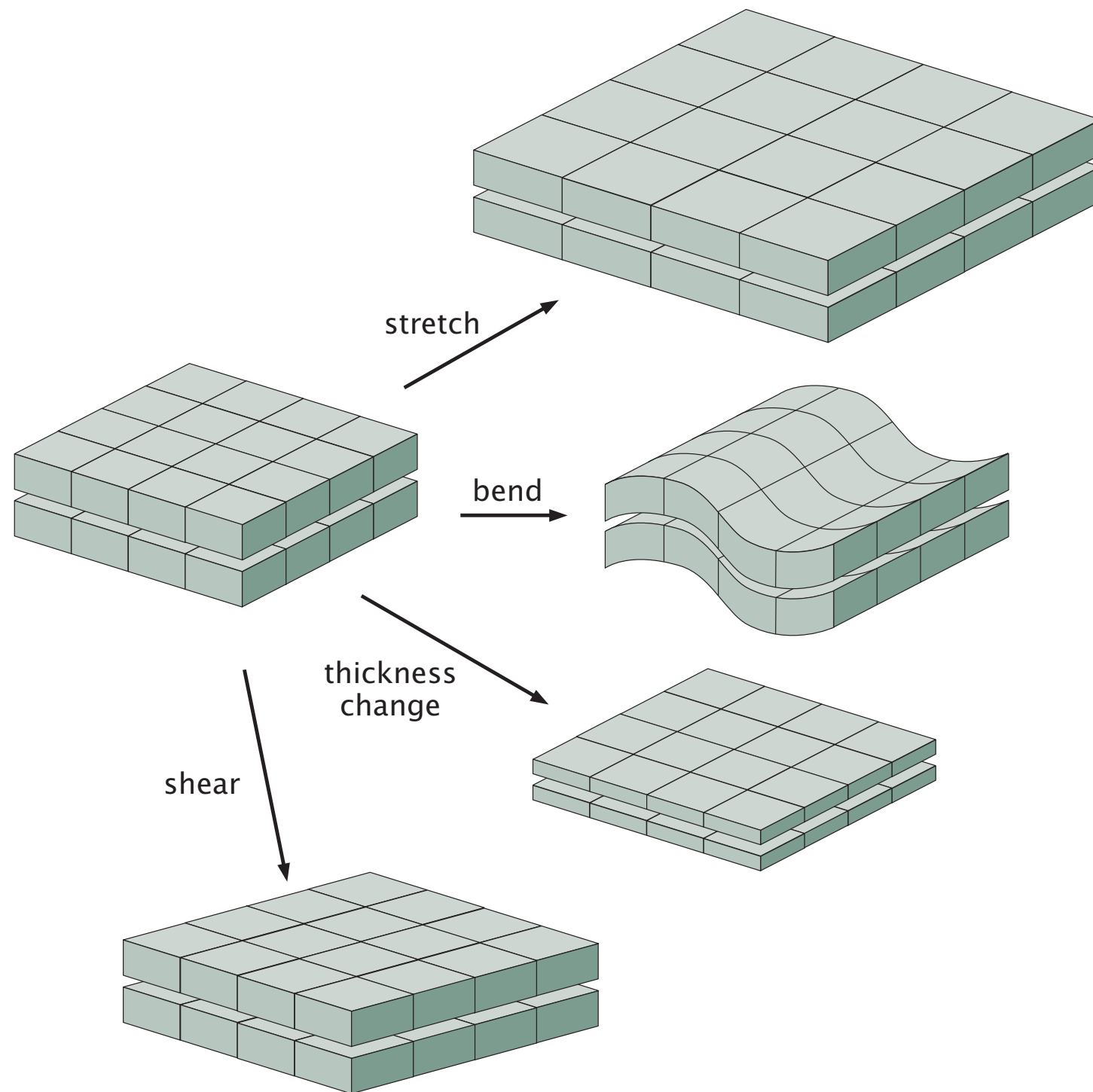


**interactions between
coat proteins bend
the membrane**



**insertions of protein parts
between lipid molecules
on one side of the layer**

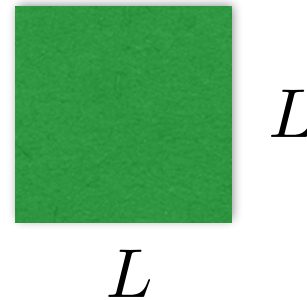
Membrane deformations



R. Phillips et al., Physical
Biology of the Cell

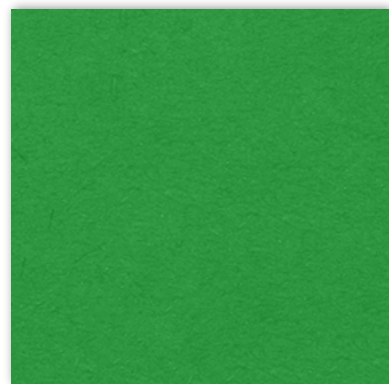
Energy cost for stretching and shearing

undeformed
square patch



patch area
 $A = L^2$

isotropic
deformation



$L + \Delta L$

$L + \Delta L$

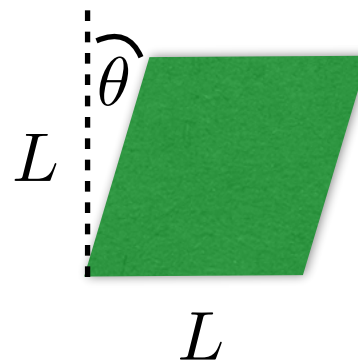
$$\frac{E}{A} = \frac{B}{2} \left(\frac{\Delta A}{A} \right)^2 \approx \frac{B}{2} \left(\frac{2\Delta L}{L} \right)^2$$

bulk modulus

$$B \sim 0.2 \text{ N/m}$$

(lipid bilayer)

shear
deformation



$$\frac{E}{A} = \frac{\mu \theta^2}{2}$$

shear modulus

$$\mu \sim 10^{-5} \text{ N/m}$$

(spectrin network)

anisotropic
stretching



$L(1 + \lambda_2)$

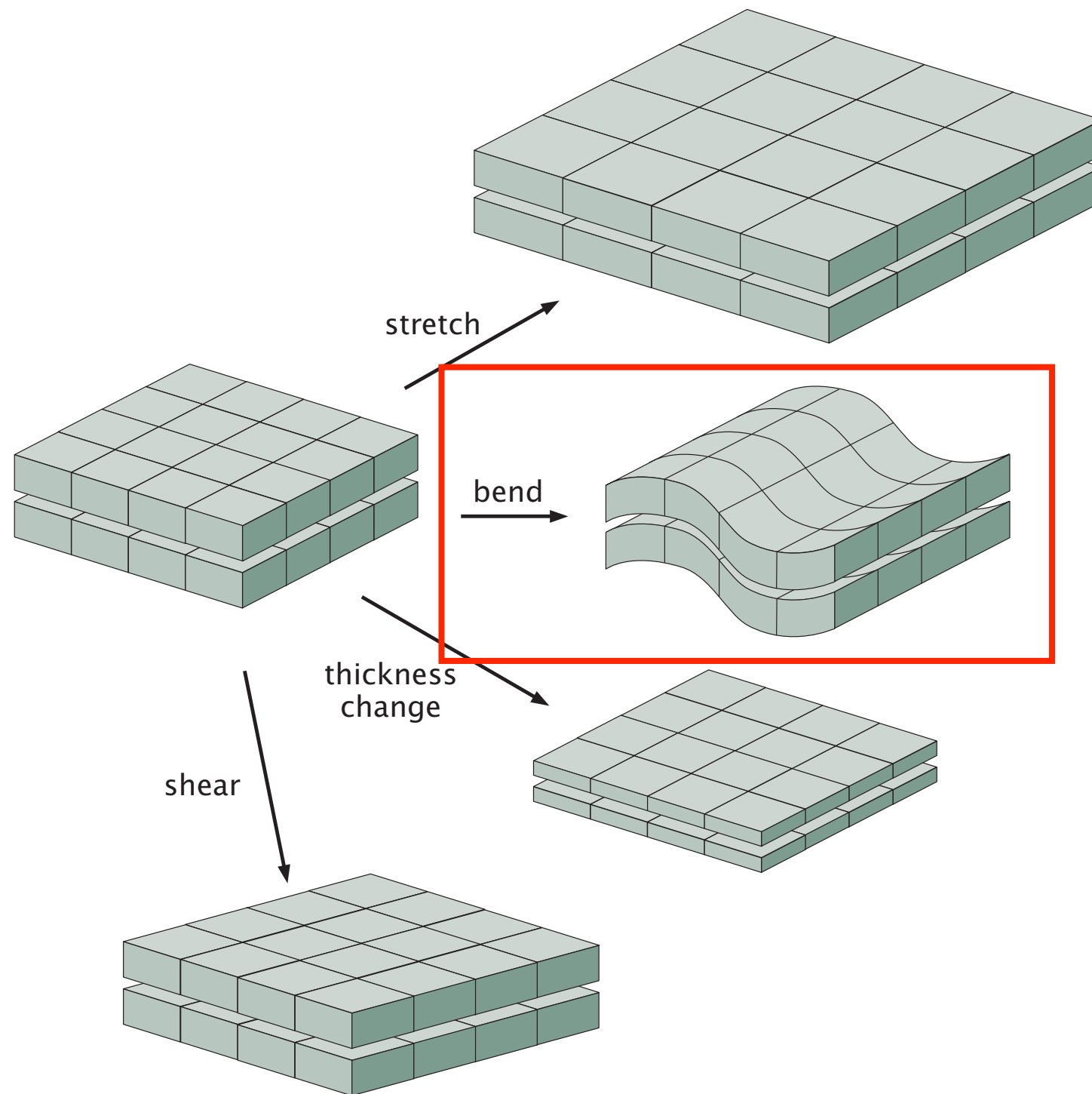
$L(1 + \lambda_1)$

$$\frac{E}{A} \approx \frac{B}{2} (\lambda_1 + \lambda_2)^2 + \frac{\mu}{2} (\lambda_1 - \lambda_2)^2$$

$$\lambda_1, \lambda_2 \ll 1$$

(shearing can be interpreted
as anisotropic stretching)

Membrane deformations



R. Phillips et al., Physical
Biology of the Cell

Bending energy

$$E = \int dA \left[\frac{\kappa}{2} \left(\frac{1}{R_1} + \frac{1}{R_2} - C_0 \right)^2 + \frac{\kappa_G}{R_1 R_2} \right]$$

**Helfrich
free energy**

bending rigidity $\kappa \sim 20k_B T$

mean curvature $H = \frac{1}{2} \left(\frac{1}{R_1} + \frac{1}{R_2} \right)$

**Gaussian
bending rigidity** $\kappa_G \sim -0.8\kappa$

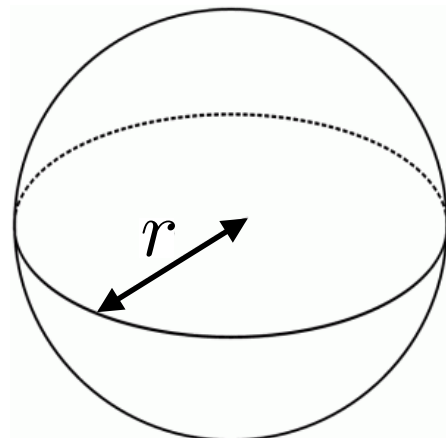
**Gaussian
curvature** $G = \frac{1}{R_1 R_2}$

**spontaneous
curvature** C_0

Example: bending energy for a sphere

$$\frac{1}{R_1} = \frac{1}{R_2} = \frac{1}{r}$$

$$C_0 = 0$$



$$E = 4\pi (2\kappa + \kappa_G) \sim 300k_B T$$

**bending energy is independent
of the sphere radius!**

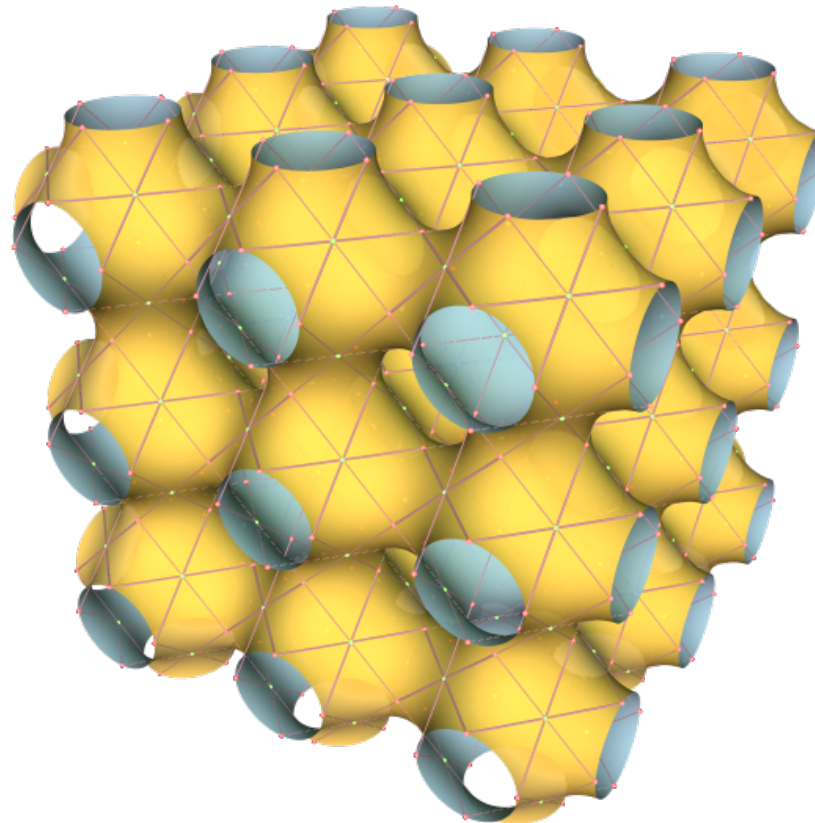
Bending energy

$$E = \int dA \left[\frac{\kappa}{2} \left(\frac{1}{R_1} + \frac{1}{R_2} - C_0 \right)^2 + \frac{\kappa_G}{R_1 R_2} \right]$$

Gaussian bending rigidity κ_G has to be negative for stability of membranes

Schwarz minimal surface

Such surfaces would be preferred for positive Gaussian bending rigidity, when $C_0=0$.



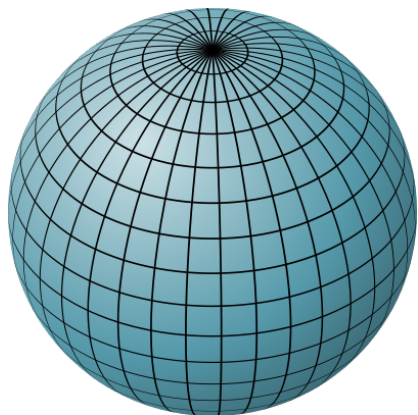
$$\frac{1}{R_1} + \frac{1}{R_2} = 0$$
$$\frac{1}{R_1 R_2} < 0$$

Gauss-Bonnet theorem

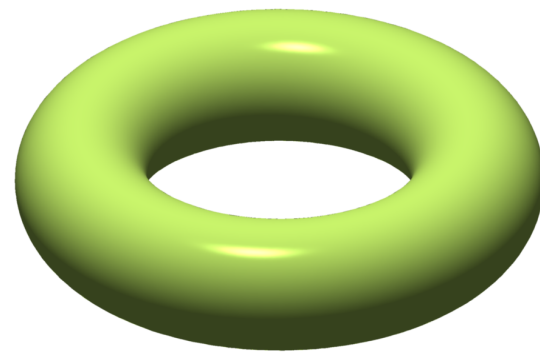
For closed surfaces the integral over Gaussian curvature only depends on the surface topology!

$$\int \frac{dA}{R_1 R_2} = 4\pi (1 - g)$$

$g = 0$



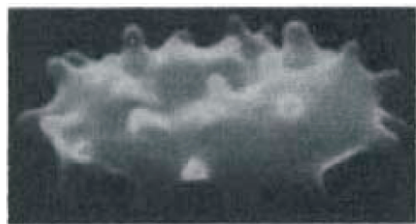
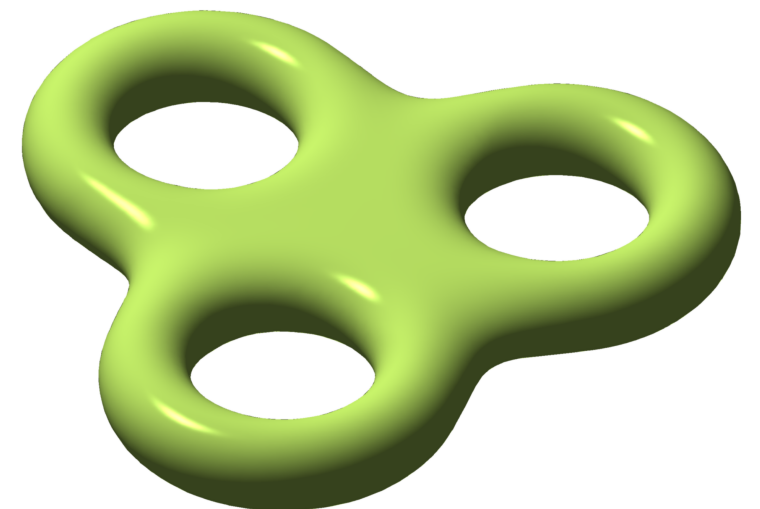
$g = 1$



$g = 2$

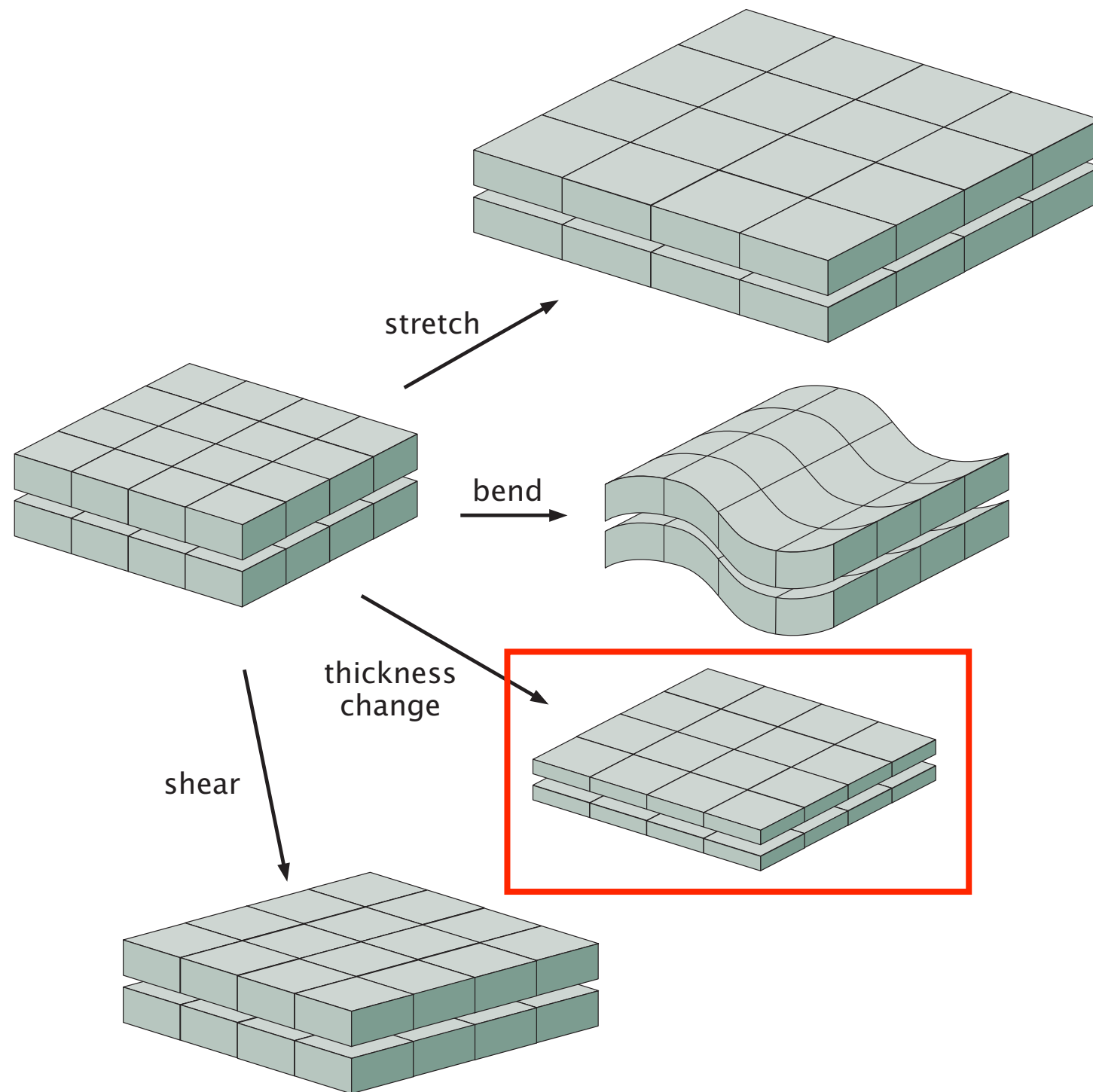


$g = 3$



It is hard to experimentally measure the Gaussian bending rigidity for cells, because cell deformations don't change the topology!

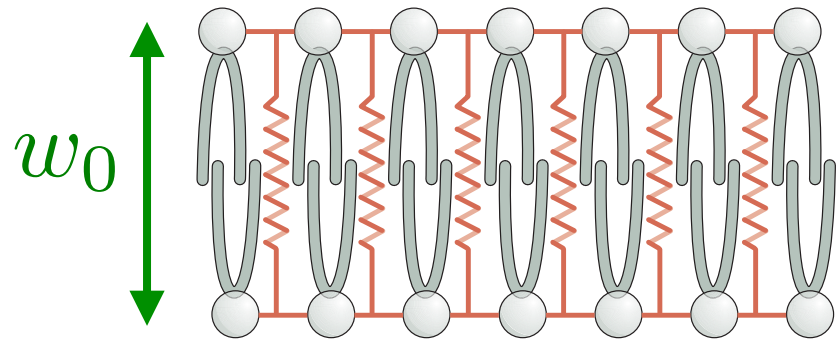
Membrane deformations



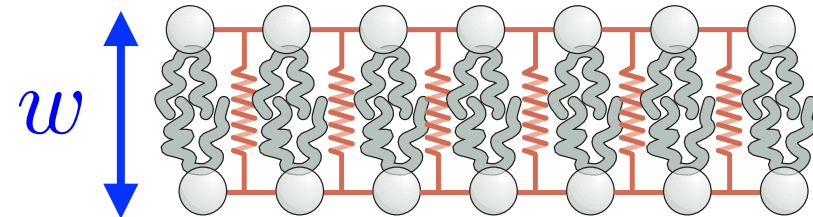
R. Phillips et al., Physical
Biology of the Cell

Membrane thickness deformation

undeformed bilayer



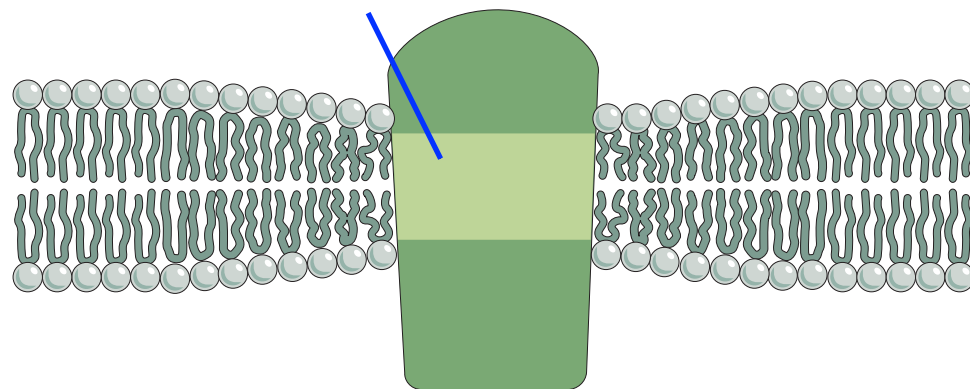
deformed bilayer



$$E_t = \frac{K_t}{2} \int dA \left(\frac{w - w_0}{w_0} \right)^2$$

$$K_t \approx 60k_B T / \text{nm}^2$$

hydrophobic region
of protein



**Membrane proteins can
locally deform the
thickness of lipid bilayer**

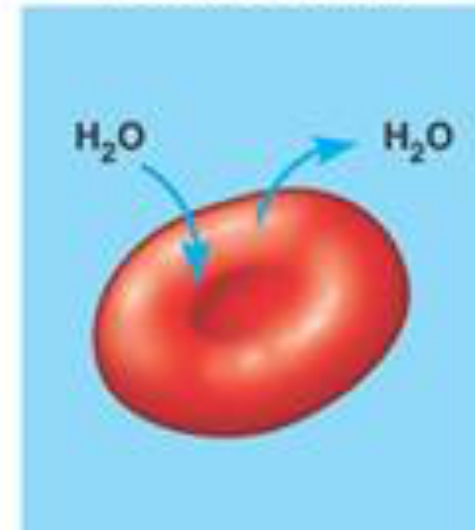
Osmotic pressure in cells

If extracellular solution has different concentration of ions from the interior of cells, then the resulting flow of water can cause the cell to shrink or swell and even burst.



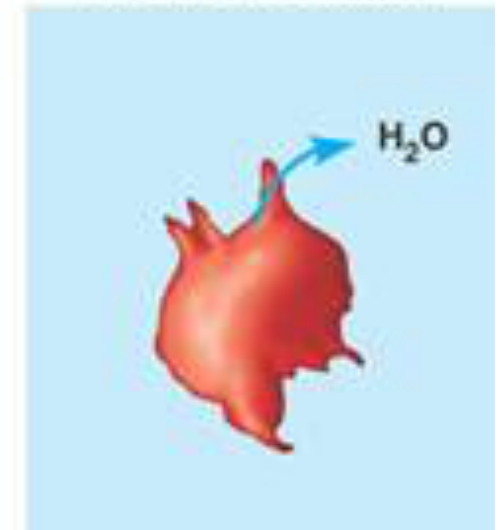
hypotonic
solution

$$C_{s,out} \ll C_{s,in}$$



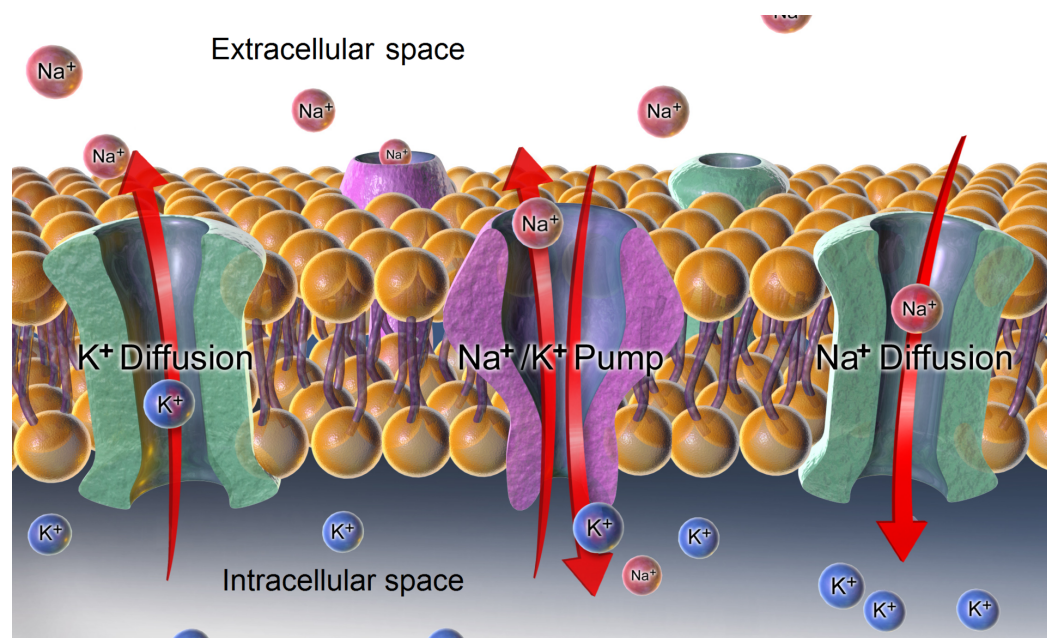
isotonic
solution

$$C_{s,out} \sim C_{s,in}$$



hypertonic
solution

$$C_{s,out} \gg C_{s,in}$$



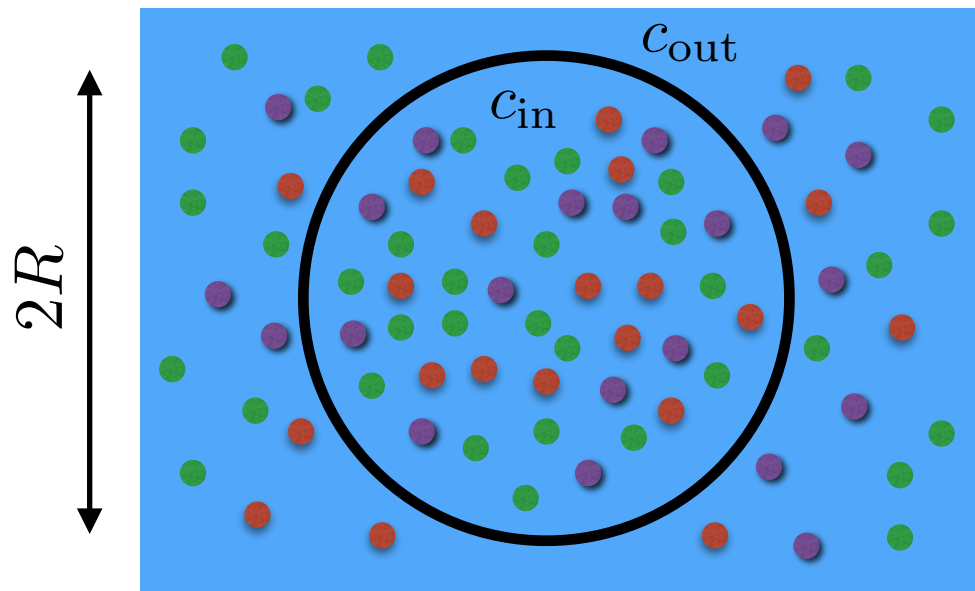
Cells use ion channels and ion pumps to regulate concentration of ions and therefore also the cell volume.

(Note: cell membrane is impermeable for charged particles)

Osmotic pressure

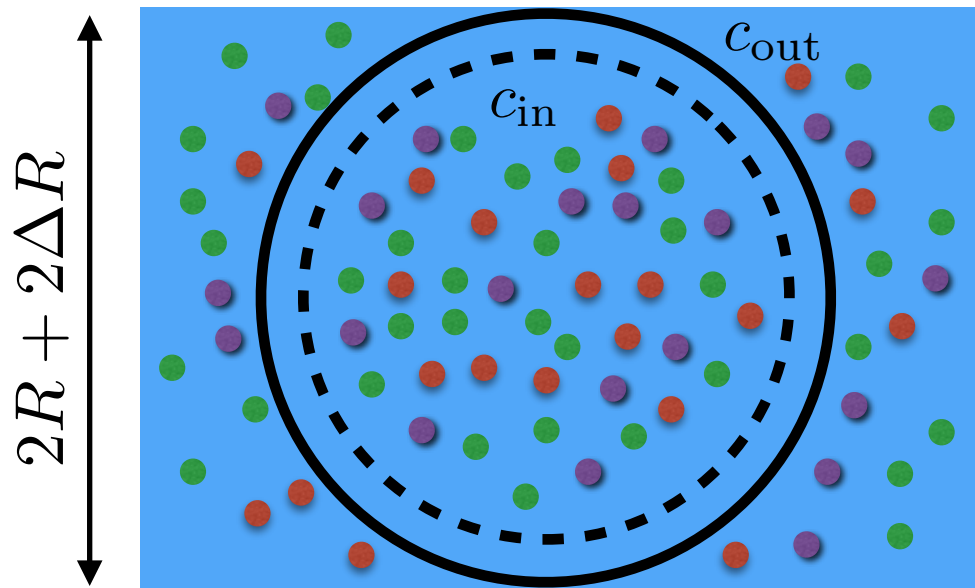
$$\Delta p = p_{\text{in}} - p_{\text{out}} = k_B T (c_{\text{in}} - c_{\text{out}})$$

$$c_{\text{in}} > c_{\text{out}}$$



Water flows in the cell until the mechanical equilibrium is reached.

$$c_{\text{in}} > c_{\text{out}}$$



The radius of swollen cell can be estimated by minimizing the vesicle energy.

$$A = 4\pi R^2$$

$$V = \frac{4\pi R^3}{3}$$

$$E = A \frac{B}{2} \left(\frac{\Delta A}{A} \right)^2 - \Delta p \Delta V$$

$$E = 8\pi B \Delta R^2 - 4\pi R^2 \Delta p \Delta R$$

$$\frac{\Delta R}{R} = \frac{R \Delta p}{4B}$$

Membrane tension

$$\tau = B \frac{\Delta A}{A} = B \frac{2\Delta R}{R} = \frac{R \Delta p}{2}$$

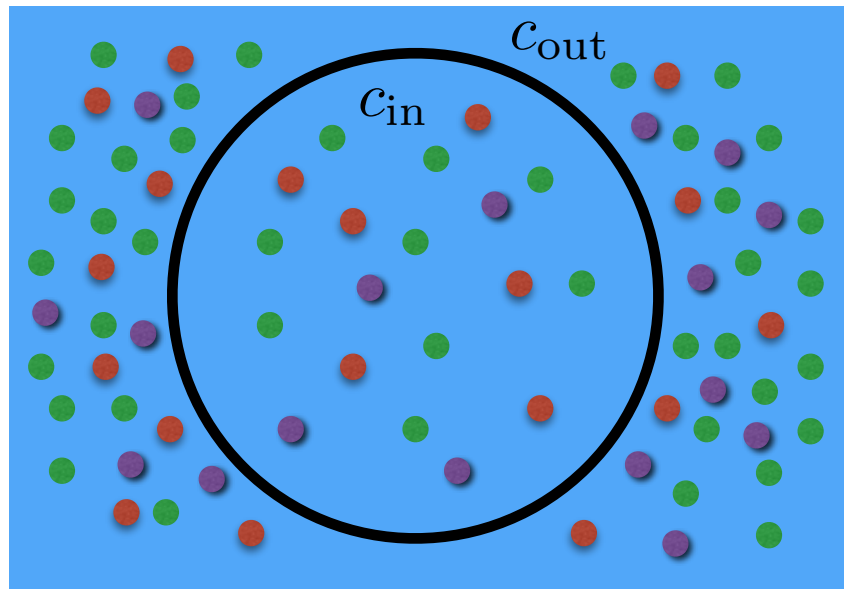
(Young-Laplace equation)

$$\Delta p = \tau (1/R_1 + 1/R_2)$$

Osmotic pressure

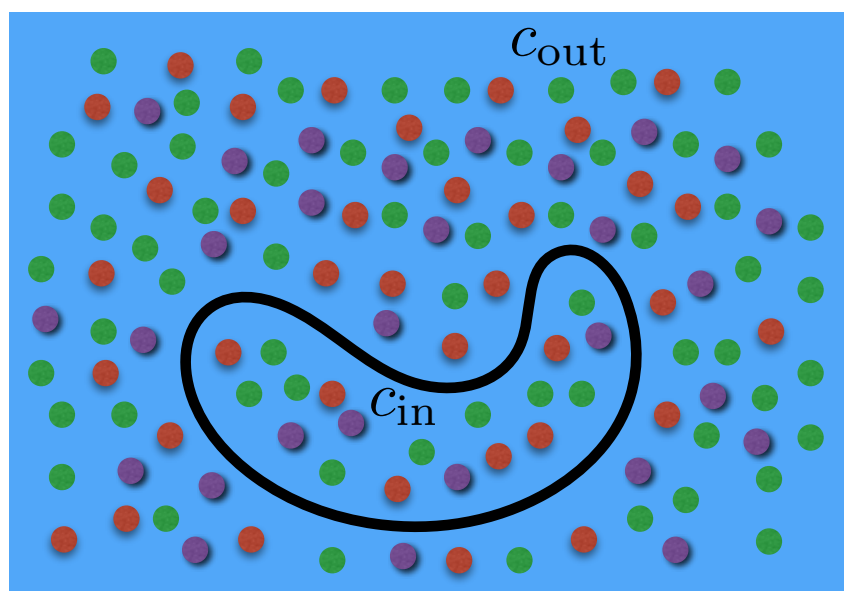
$$\Delta p = p_{\text{in}} - p_{\text{out}} = k_B T (c_{\text{in}} - c_{\text{out}})$$

$$c_{\text{in}} < c_{\text{out}}$$



Water flows out of the cell until concentrations become equal.

$$c_{\text{in}} = c_{\text{out}}$$



How can we estimate the shape of “deflated” cells?

Total concentration of molecules inside a cell (vesicle)

$$c_{\text{in}} = \frac{N}{V}$$

Preferred cell (vesicle) volume

$$V_0 = \frac{N}{c_{\text{out}}}$$

Energy cost for modifying the volume

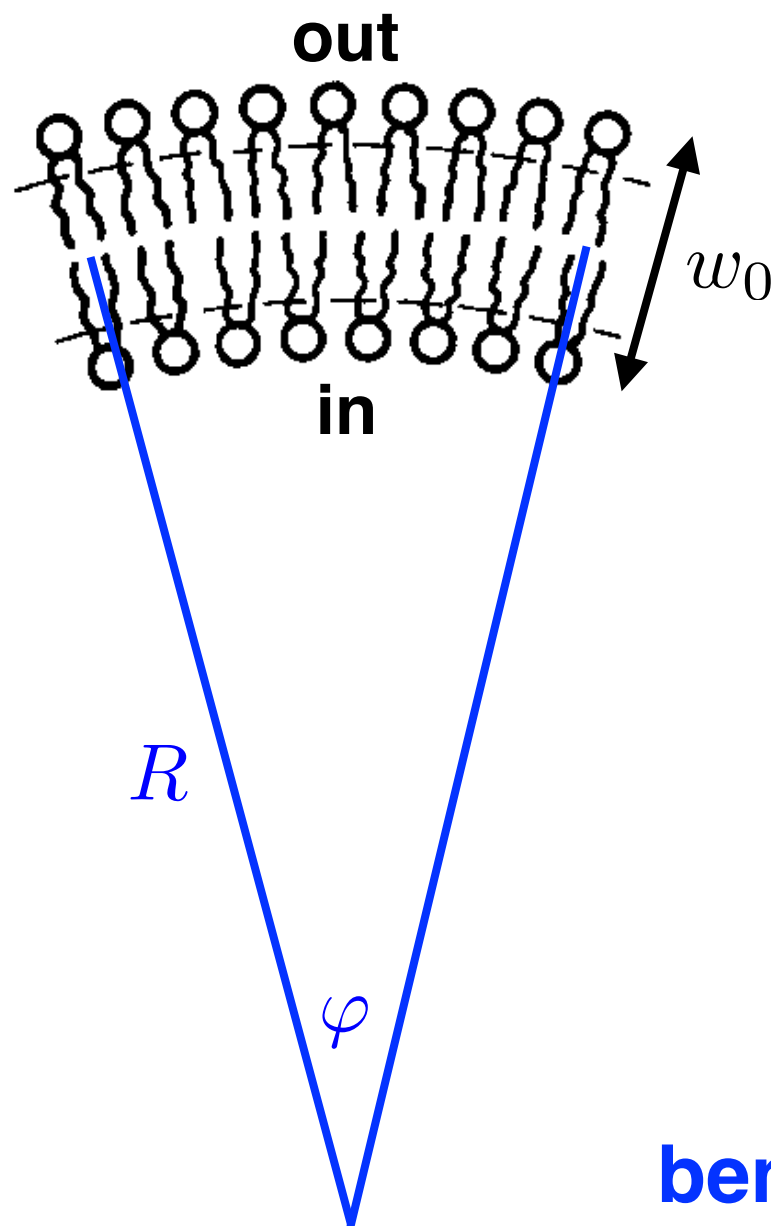
$$E_v = - \int_{V_0}^V \Delta p(V) dV$$

$$E_v = -k_B T \left[N \ln \left(\frac{V}{V_0} \right) - c_{\text{out}} (V - V_0) \right]$$

$$E_v = \frac{1}{2} k_B T c_{\text{out}} V_0 \left(\frac{V - V_0}{V_0} \right)^2$$

Area difference between lipid layers

Length difference for 2D example on the left



$$\Delta \ell = \ell_{\text{out}} - \ell_{\text{in}} = (R + w_0/2)\varphi - (R - w_0/2)\varphi$$

$$\Delta \ell = w_0 \varphi = \frac{w_0 \ell}{R}$$

Area difference between lipid layers in 3D

$$\Delta A = A_{\text{out}} - A_{\text{in}} = w_0 \int dA \left(\frac{1}{R_1} + \frac{1}{R_2} \right)$$

Lipids can move within a given layer, but flipping between layers is unlikely. This sets a preferred area difference ΔA_0 .

Non-local bending energy

$$E = \frac{k_r}{2Aw_0^2} (\Delta A - \Delta A_0)^2$$

$$k_r \approx 3\kappa \approx 60k_B T$$

Total elastic energy for cells (vesicles)

Shape of cells (vesicles) can be obtained by minimizing the total elastic energy

this term is constant for a given topology

$$E = \int dA \left[\frac{1}{2} (B - \mu) u_{ii}^2 + \mu u_{ij}^2 + \frac{\kappa}{2} \left(\frac{1}{R_1} + \frac{1}{R_2} - C_0 \right)^2 + \frac{\kappa_G}{R_1 R_2} \right] + \frac{k_r}{2A_0 w_0^2} (\Delta A - \Delta A_0)^2 + \frac{1}{2} k_B T c_{\text{out}} V_0 \left(\frac{V - V_0}{V_0} \right)^2$$

Energetically it is very costly to change the cell volume V_0 and the membrane area A_0 (large bulk modulus B)!

Introduce dimensionless quantities that would be equal to 1 for sphere

definition for sphere radius

$$R_0 = \sqrt{\frac{A_0}{4\pi}}$$

dimensionless area

$$a = \frac{A_0}{4\pi R_0^2} = 1$$

dimensionless volume

$$v = \frac{V_0}{4\pi R_0^3/3}$$

dimensionless curvature

$$c_0 = C_0 R_0$$

dimensionless area difference between layers

$$\Delta a = \frac{\Delta A_0}{8\pi w_0 R_0}$$

dimensionless energy

$$e = \frac{E}{8\pi\kappa}$$

Minimal model: minimization of bending energy for lipid vesicles

Find the shape of vesicles that minimize bending energy by constraining the volume to $v < 1$.

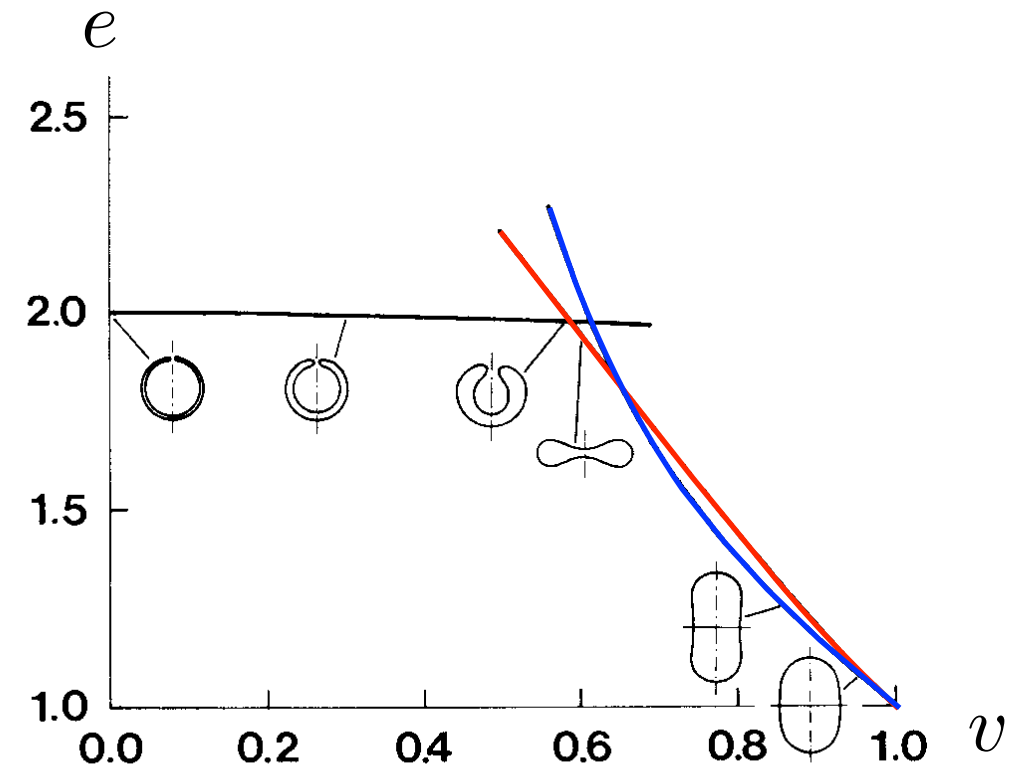
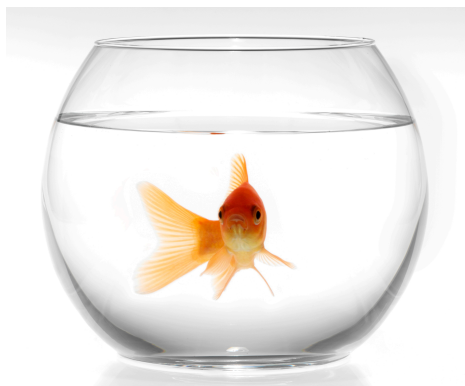
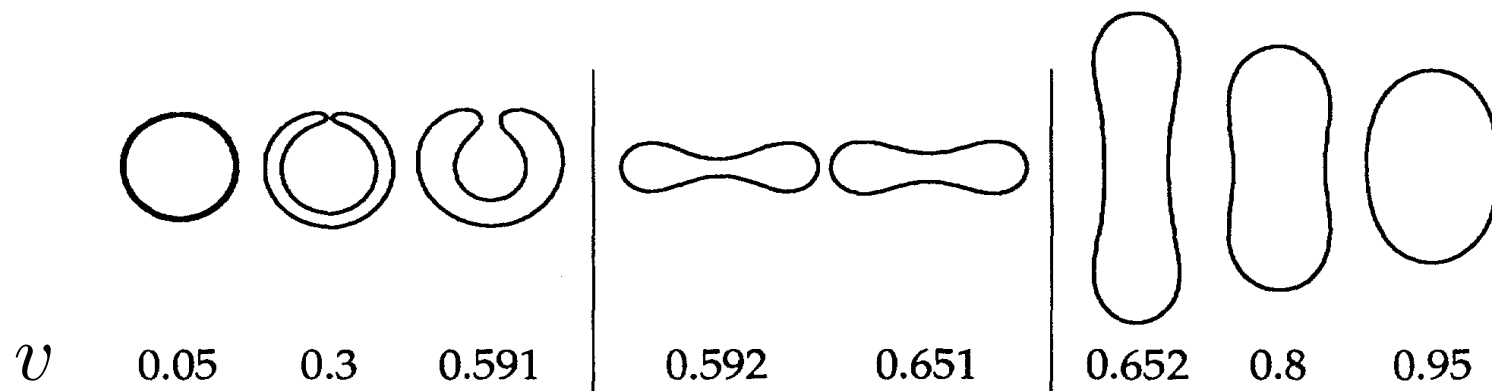
$$e = \int \frac{da}{4} \left(\frac{1}{r_1} + \frac{1}{r_2} \right)^2$$

Minimum energy configurations

stomatocytes

oblates

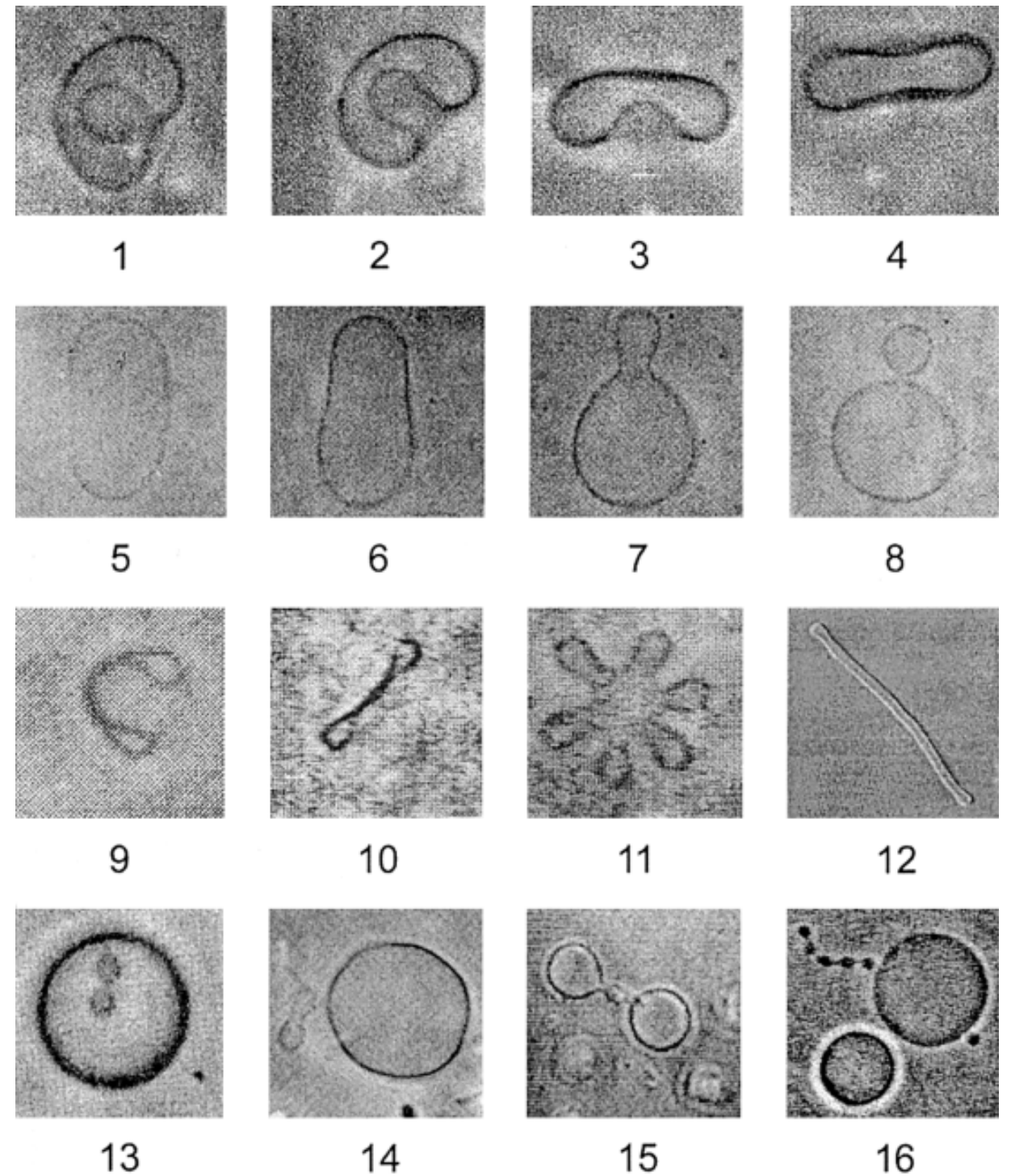
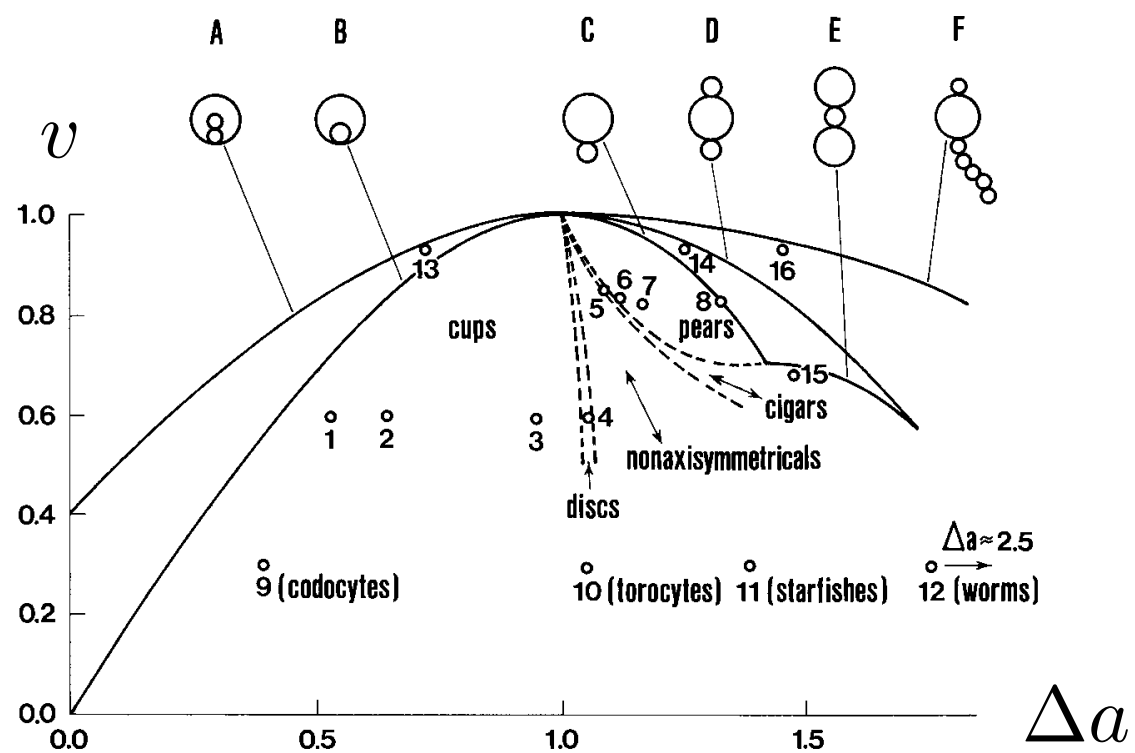
prolates



Bilayer couple model of vesicles

$$e = \int \frac{da}{4} \left(\frac{1}{r_1} + \frac{1}{r_2} - c_0 \right)^2 + \frac{k_r}{\kappa} (\Delta a - \Delta a_0)^2$$

Phase diagram of vesicle shapes that minimize the free energy for $c_0 = 0$, $k_r/\kappa \rightarrow \infty$.



S. Svetina and B. Zeks,
Anat. Rec. 268, 215 (2002)